Nuclear imaging
PET, SPECT

J. Kybic

Department of cybernetics, FEE CTU
http://cmp.felk.cvut.cz/~kybic
kybic@fel.cvut.cz

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Resources

- http://www.bic.mni.mcgill.ca/~louis/seminars/399-650/pet.html
- http://ocw.mit.edu/NR/rdonlyres/Nuclear-Engineering/22-01Introduction-to-Ionizing-RadiationFall2003/60AA5867-88AE-49C7-9478-2F4661B4EBBE/0/pet_spect.pdf
- http://www.pet.mc.duke.edu/rsna04/turk-petspectphysicsRSNA2005.pdf
- http://www.nuclear.kth.se/courses/medphys/5A1414/TOFPET1.pdf
- http://www.fmri.org,
- A. Webb: Introduction to Biomedical Imaging
- images by: Wikipedia, NIH, Moazemi et al., Rager et al., Virginia Commonwealth University. . .

Principles of nuclear imaging

Radioactivity

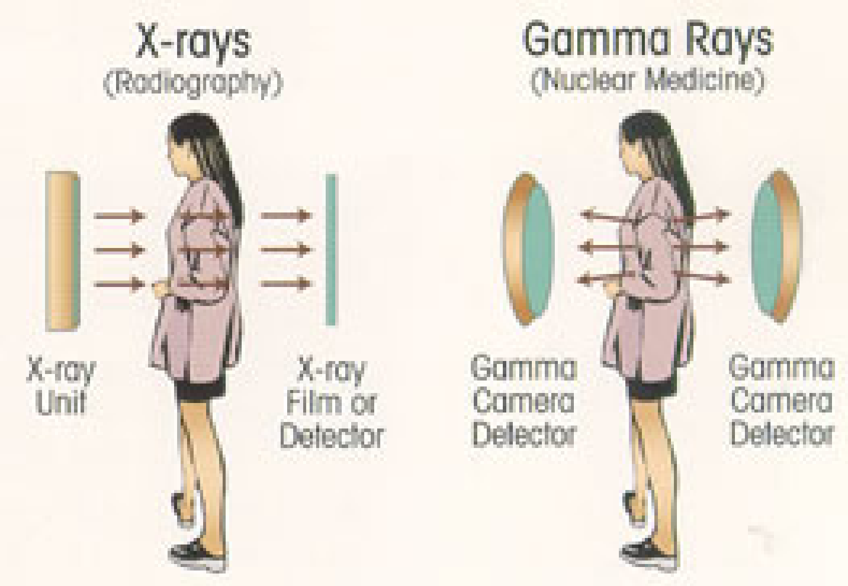
Gamma camera

SPECT

PET

Conclusions

Nuclear versus X-ray imaging



Nuclear versus X-ray imaging (2)

- **X-ray and CT**
  - *transmission* imaging, external source
- **PET, SPECT**
  - *emission* imaging, source internal to body

Nuclear versus X-ray imaging (2)

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  - Anatomic imaging (shape, fracture)
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  - Functional imaging (metabolism, perfusion), tracer concentration

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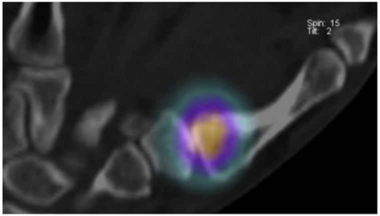
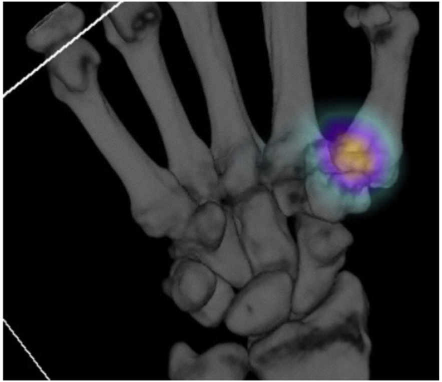
  - Functional imaging (metabolism, perfusion), tracer concentration
  - γ rays

Nuclear versus X-ray imaging (2)

- **X-ray and CT**
  - *transmission* imaging, external source
  - Anatomic imaging (shape, fracture)
  - X-rays
  - Good resolution, $< 1\,\text{mm}$
- **PET, SPECT**
  - *emission* imaging, source internal to body
  - Functional imaging (metabolism, perfusion), tracer concentration
  - γ rays
  - Lower resolution, $5 \sim 20\,\text{mm}$

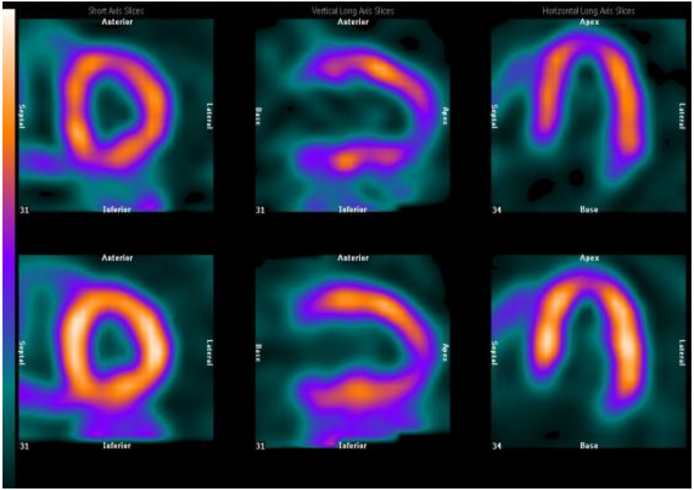
Nuclear imaging applications





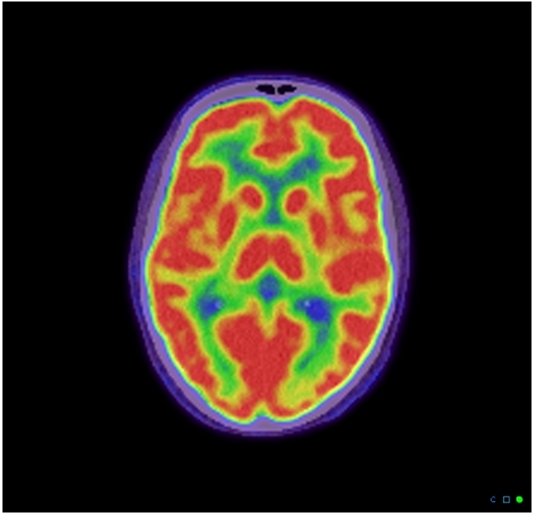
Hand, osteoarthritis, CT+SPECT

Nuclear imaging applications



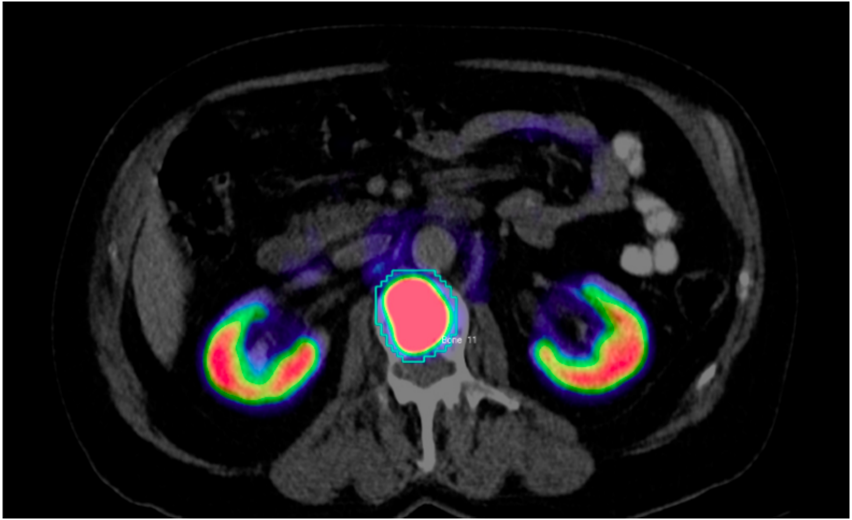
Heart, myocardial perfusion, PET

Nuclear imaging applications



Brain, FDG PET, metabolism

Nuclear imaging applications



Renal (kidney) PET+CT, Ga-PSMA contrast agent.

Nuclear imaging applications

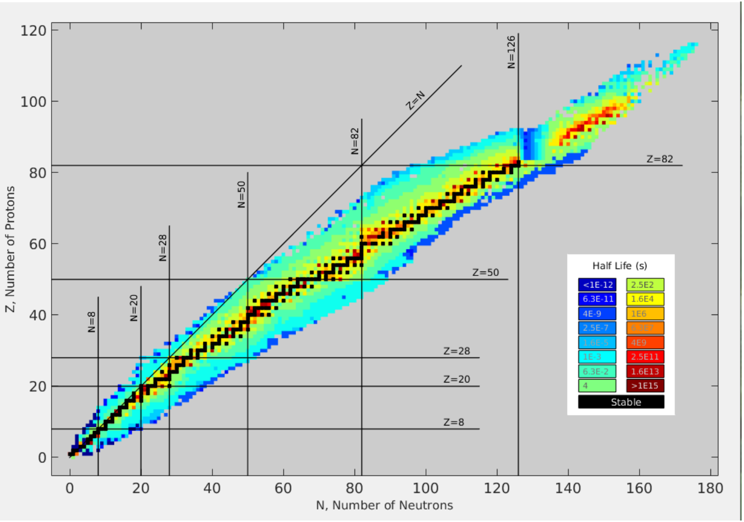


Metastases, SPECT+CT, MIP

Radioactivity

- element = same number of protons
- isotope/nuclide = same number of protons and neutrons
- excess of neutrons/protons → instability → radioactive decay chain → stable isotope

Valley of stability



Isotopes with Z slightly smaller than N are stable.

Radioactive decay modes

$$\text{Unstable parent nucleus} \longrightarrow \text{Daughter nucleus} + \text{particles (energy)}$$

- Alpha decay (α)
- Beta decay (β)
- Positron decay (β^+)
- Isomeric transition
- Electron capture
- *Proton emission, neutron emission, ...*

Alpha decay

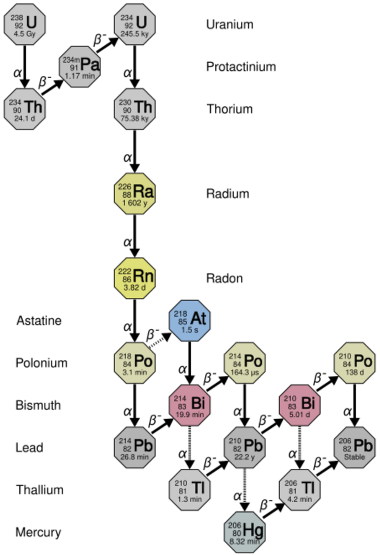
- Spontaneous emission of α particles
  - 2 protons + 2 neutrons, ${}^4_2\text{He}$, charged
  - energy $4 \sim 8\,\text{MeV}$, speed $0.05c$
  - strong interaction, low penetration (cm in air, μm in tissue), easy shielding
  - important biological effects (relative biological effectiveness 20), DNA damage
  - no use in imaging, used in therapy
- happens in heavy nuclei (radium, polonium, uranium, thorium, radon, ...) and Be
- excess energy released as γ (electromagnetic) rays (photons)

$$ {}^A_Z\text{X} \xrightarrow{\alpha} {}^{A-4}_{Z-2}\text{Y} + \underbrace{{}^4_2\text{He}}_{\alpha} $$

$$ \underbrace{{}^{226}_{88}\text{Ra}}_{\text{radium}} \xrightarrow{\alpha} \underbrace{{}^{222}_{86}\text{Rn}}_{\text{radon}} + \underbrace{{}^4_2\text{He}}_{\alpha} $$

$$ {}^{222}_{86}\text{Rn} \xrightarrow{\alpha} {}^{218}_{84}\text{Po} \xrightarrow{\alpha} \ldots \longrightarrow {}^{206}_{82}\text{Pb} $$

Decay chain



238 92 U 4.5 Gy
234m 91 Pa 1.17 min
234 92 U 245.5 ky
234 90 Th 24.1 d
230 90 Th 75.38 ky
226 88 Ra 1 602 y
222 86 Rn 3.82 d
218 85 At 1.5 s
218 84 Po 3.1 min
214 84 Po 164.3 μs
210 84 Po 138 d
214 83 Bi 19.9 min
210 83 Bi 5.01 d
214 82 Pb 26.8 min
210 82 Pb 22.2 y
206 82 Pb Stable
210 81 Tl 1.3 min
206 81 Tl 4.2 min
206 80 Hg 8.32 min
α
β⁻
Uranium
Protactinium
Thorium
Radium
Radon
Astatine
Polonium
Bismuth
Lead
Thallium
Mercury

Beta decay

- β particles = electrons e^-
- Neutron conversion

$$n \xrightarrow{\beta} p + e^- + \bar{\nu}_e$$

$\bar{\nu}_e$ — electron antineutrino

$$^{A}_{Z}X \xrightarrow{\beta} {}^{A}_{Z+1}Y + e^- + \bar{\nu}_e$$

- For neutron-rich $(N > Z)$ isotopes
- e^- ejected with high energy (β rays), continuous spectrum
- remaining energy = $\bar{\nu}_e$, nucleus recoil
- excited state nucleus $\longrightarrow \gamma$ rays

Beta decay

Examples

$$^{14}_{6}\text{C} \xrightarrow{\beta} {}^{14}_{7}\text{N} + \text{e}^- + \bar{\nu}_e \qquad \text{half-life 5730 years}$$

$$^{99}_{42}\text{Mo} \xrightarrow{\beta} {}^{99m}_{43}\text{Tc} + \text{e}^- + \bar{\nu}_e \qquad \text{half-life 2.7 days}$$

Isomeric transition

Excited state nucleus $\longrightarrow \gamma$ rays

Metastable **Technetium** ${}^{99m}_{43}\text{Tc}$

$${}^{98}_{42}\text{Mo} \longrightarrow {}^{99}_{42}\text{Mo} \qquad \text{neutron bombardment}$$

$${}^{99}_{42}\text{Mo} \xrightarrow{\beta} {}^{99m}_{43}\text{Tc} + e^- + \bar{\nu}_e \qquad \text{half-life 2.7 days}$$

$$\boxed{{}^{99m}_{43}\text{Tc} \xrightarrow{\gamma} {}^{99}_{43}\text{Tc}} \qquad \text{half-life 6 h}$$

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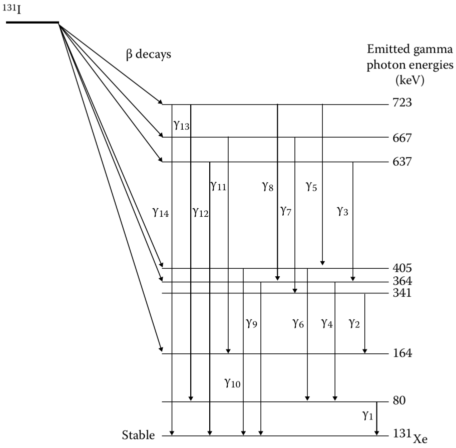
$${}^{99}_{43}\mathrm{Tc} \xrightarrow{\beta} {}^{99}_{44}\mathrm{Ru} \qquad \text{half-life} > 200\,000 \text{ years}$$

- most commonly used medical radioisotope
- γ (photon) energy 140 keV

Multiple decay processes

Iodine



Positron decay

β^+ decay

- β^+ particles = positrons e^+
- Proton conversion

$$p \xrightarrow{\beta^+} n + e^+ + \nu_e$$

ν_e — electron neutrino

$$^A_Z\mathrm{X} \xrightarrow{\beta^+} {}^{A}_{Z-1}\mathrm{Y} + e^+ + \nu_e$$

- For proton-rich $(N < Z)$ isotopes

Positron decay

β^+ decay

Examples

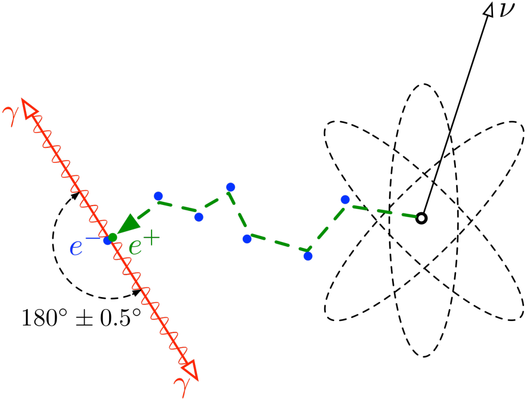
$$^{23}_{12}\mathrm{Mg} \xrightarrow{\beta^+} {}^{23}_{11}\mathrm{Na} + \mathrm{e}^+ + \nu_e \qquad \text{half-life } 11\,\mathrm{s}$$

$$^{68}_{31}\mathrm{Ga} \xrightarrow{\beta^+} {}^{68}_{30}\mathrm{Zn} + \mathrm{e}^+ + \nu_e \qquad \text{half-life } 68\,\mathrm{min}$$

Positron decay

β^+ decay

- Positron e^+ is **annihilated**: $e^+ + e^+ \longrightarrow \gamma + \gamma$



e^+ positron

e^- electron

ν neutrino

γ quantum/photon (511 keV)

- **two photons** with energy 511 keV
- Parent/daughter nuclide energy difference $\gtrsim 1$ MeV

Electron capture

- Proton absorbs inner electron

$$p + e^- \xrightarrow{\text{EC}} n + \nu_e$$

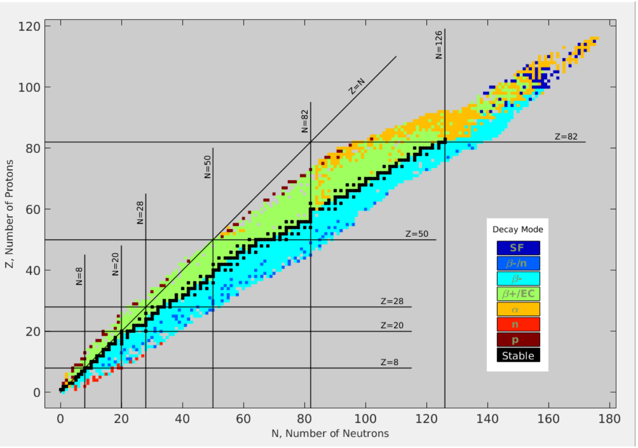
$$^{A}_{Z}X + e^- \xrightarrow{\text{EC}} {}^{A}_{Z-1}Y + \nu_e$$

Example:

$$\underbrace{^{51}_{24}\text{Cr}}_{\text{chromium}} + e^- \xrightarrow{\text{EC}} \underbrace{^{51}_{23}\text{V}}_{\text{vanadium}} + \nu_e$$

- Neutrino carries all energy (characteristic spectrum)
- Can occurr for smaller energy differences
- Excited state nucleus $\longrightarrow \gamma$ rays

Decay mode chart



black: stable, light blue: β, green: β^+ or electron capture, orange: α, dark blue: fission, red: neutron emission, brown: proton emission

Nuclear imaging methods

- **SPECT**
  - γ camera (2D)
  - single photon emission computed tomography (3D)
  - γ photon emitters
- **PET**
  - positron emission tomography (3D)
  - positron emitters

Ideal radionuclides for SPECT imaging

- Physical half-life long enough to allow preparation
- Physical half-life short enough to minimize long-term effects
- Pure γ emitter (isomeric transition, electron capture)
- Photon energy high-enough to penetrate tissue
- Photon energy low-enough for efficient shielding and detection

Single photon emitters

for SPECT nuclear imaging

Nuclide		Half-life	E_{photon} [keV]	
Technetium	$^{99m}_{43}\text{Tc}$	6 h	140	most used
Iodine	$^{123}_{53}\text{I}$	13 h	159	thyroid imaging
Indium	$^{111}_{53}\text{In}$	2.8 d	171, 245	good, expensive
Thallium	$^{201}_{81}\text{Tl}$	3 d	$70 \sim 80$	cardiac perfussion
Gallium	$^{67}_{31}\text{Ga}$	3.25 d	$90 \sim 400$	tumor localization
Iodine	$^{131}_{53}\text{I}$	8.1 d	$364 \sim 606$	radiotherapy

Positron emitters

for PET nuclear imaging

Nuclide		Half-life	
Rubidium	$^{82}_{37}\mathrm{Rb}$	1.3 min	cardiac imaging
Oxygen	$^{15}_{8}\mathrm{O}$	2 min	
Nitrogen	$^{13}_{7}\mathrm{N}$	10 min	
Carbon	$^{11}_{6}\mathrm{C}$	20.3 min	
Gallium	$^{68}_{31}\mathrm{Ga}$	68 min	tumor localization
Fluorine	$^{18}_{9}\mathrm{F}$	110 min	most often used, FDG
Copper	$^{64}_{35}\mathrm{Cu}$	12.7 h	oncology, radiotherapy

Mostly short half-time — need to be produced in-situ.

Activity

- Activity $A[\mathrm{Bq}]$, $1\,\mathrm{Bq} = 1\,\mathrm{desintegration/s}$,
- Older unit $1\,\mathrm{Ci} = 3.7 \cdot 10^{10}\,\mathrm{Bq}$ — 1 g of radium

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- For N nuclei and a *decay constant* λ

$$A = \lambda N = -\frac{\mathrm{d}N}{\mathrm{d}t}$$

Exponential decay

- Exponential decay of N

$$N = N_0 e^{-\lambda t}$$

Exponential decay

- Exponential decay of N

$$N = N_0 \mathrm{e}^{-\lambda t}$$

- Half-life

$$T_{1/2} = \log 2/\lambda \approx 0.693/\lambda \text{ [s]}$$

$$N = N_0 \left(\frac{1}{2}\right)^{\frac{t}{T_{1/2}}}$$

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$$N = N_0 \left(\frac{1}{2}\right)^{\frac{t}{T_{1/2}}}$$

- Exponential decay of A

$$A = A_0 \mathrm{e}^{-\lambda t}, \qquad \text{with} \quad A_0 = \lambda N_0, \quad A = \lambda N$$

Effective half-life

- Physical half-life T_p
- Biological half-life T_b
- Effective half-life T_e

$$\frac{1}{T_e} = \frac{1}{T_p} + \frac{1}{T_b}$$

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Note: $T_e < T_p$, $T_e < T_b$

Effective Half-Life

E.g., for an isotope with a 6-hr half life attached to various carrier molecules with different biological half-lives.

T_P	T_B	T_E
6 hr	1 hr	0.86 hr
6 hr	6 hr	3 hr
6 hr	60 hr	5.5 hr
6 hr	600 hr	5.9 hr

Effective Half-Life

Assume 10^6 Bq localized in a tumor site, vary T

Nuclide	Half-life (T)	λ (sec^{-1})	N
1	6 sec	0.115	8.7×10^7
2	6 min	1.75×10^{-3}	5.7×10^9
3	6 hrs	3.2×10^{-5}	3.1×10^{11}
4	6 days	1.3×10^{-6}	7.7×10^{12}
5	6 years	4×10^{-9}	2.5×10^{15}

Effective Half-Life

Assume 10^{10} atoms of radionuclide localized in a tumor site, vary T

Nuclide	Half-life (T)	λ (sec^{-1})	Activity (Bq)
1	6 sec	0.115	1.15×10^9
2	6 min	1.75×10^{-3}	1.7×10^7
3	6 hrs	3.2×10^{-5}	3.2×10^6
4	6 days	1.3×10^{-6}	1.3×10^4
5	6 years	4×10^{-9}	40

Radionuclide production

- Neutron capture
- Nuclear fission
- Radionuclide generator
- (Poisitive) ion bombardment
  - Linear accelerator
  - Cyclotron

Neutron capture

Neutron activation/neutron bombardment

- Nuclear reactor, "thermal" neutrons, low energy $0.03 \sim 100\,\mathrm{eV}$
- Yield depends on neutron flow ϕ, cross section σ, decay constant λ, amount of carrier (source) material
- Chemical/physical purification

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- Chemical/physical purification

$$\text{n} + {}^{98}_{42}\text{Mo} \longrightarrow {}^{99}_{42}\text{Mo} + \gamma$$

with proton emission

$$\text{n} + {}^{32}_{16}\text{S} \longrightarrow {}^{32}_{15}\text{P} + \text{p} \qquad \text{half-life 14 days}$$

Radionuclides produced by neutron capture

Radionuclides produced by neutron absorption.

Radionuclide	Production Reaction	Gamma-Ray Energy (keV)	Half-Life	σ (Barn)
^{51}Cr	$^{50}Cr(n, \gamma)^{51}Cr$	320	27.7 days	15.8
^{59}Fe	$^{58}Fe(n, \gamma)^{59}Fe$	1099	44.5 days	1.28
^{99}Mo	$^{98}Mo(n, \gamma)^{99}Mo$	740	66.02 h	0.13
^{131}I	$^{130}Te(n, \gamma)\ ^{131}Te \rightarrow\ ^{131}I$	364	8.04 days	0.29

Source: From Mughabghab et al., 1981.

Mostly used for radiotherapy (except $^{99}_{42}Mo$)

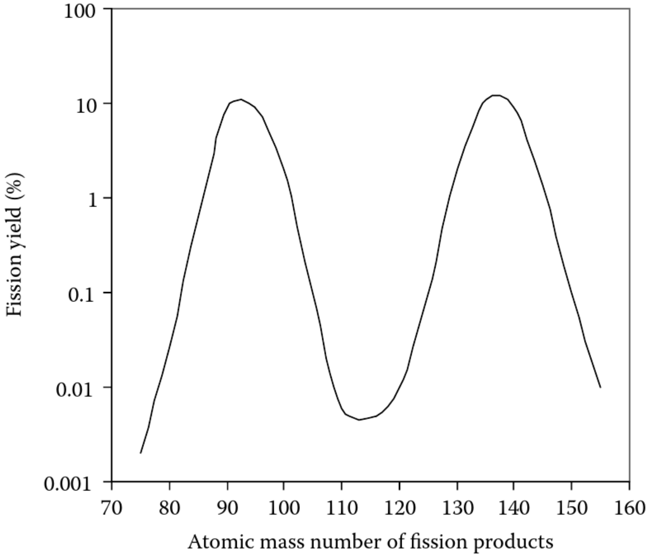
Nuclear fission

- Heavy nuclei ($A > 92$) — ${}^{235}_{92}\text{U}$, ${}^{237}_{92}\text{U}$, ${}^{239}_{94}\text{Pu}$, ${}^{232}_{90}\text{Th}$ — irradiated by neutrons $\longrightarrow$ unstable
- Fission example

$$ {}^{235}_{92}\text{U} + {}^{1}_{0}\text{n} \longrightarrow {}^{99}_{42}\text{Mo} + \underbrace{{}^{133}_{50}\text{Sn}}_{\text{tin}} + 4\,{}^{1}_{0}\text{n} $$

- Chemical/physical purification

Fission product yield for $^{235}_{92}U$



Radionuclides produced by nuclear fission

Isotope	Gamma-Ray Energy (keV)	Half-Life	Fission Yield (%)
^{99}Mo	740	66.02 h	6.1
^{131}I	364	8.05 days	2.9
^{133}Xe	81	5.27 days	6.5
^{137}Cs	662	30 a	5.9

Source: From BRH, 1970.

Radionuclide generator

- Long half-time parent isotope
- Short half-time daughter isotope, $\lambda_2 > \lambda_1$

Radionuclide generator

- Long half-time parent isotope
- Short half-time daughter isotope, $\lambda_2 > \lambda_1$
- Daughter activity (for $A_{20} = 0$)

$$A_2 = \frac{\lambda_2}{\lambda_2 - \lambda_1} A_{10} \left(\mathrm{e}^{-\lambda_1 t} - \mathrm{e}^{-\lambda_2 t} \right)$$

Radionuclide generator

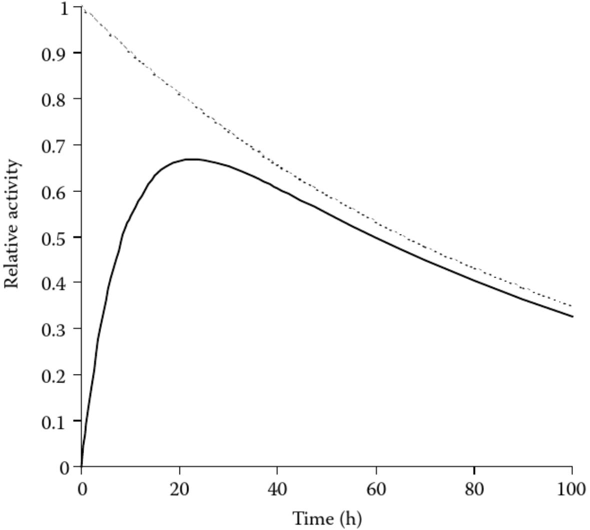
- Long half-time parent isotope
- Short half-time daughter isotope, $\lambda_2 > \lambda_1$
- Daughter activity (for $A_{20} = 0$)

$$A_2 = \frac{\lambda_2}{\lambda_2 - \lambda_1} A_{10} \left(\mathrm{e}^{-\lambda_1 t} - \mathrm{e}^{-\lambda_2 t} \right)$$

- After $\sim 10\, T_{1/2}^{(2)}$, **transient equilibrium**

$$A_1 = A_{10} \mathrm{e}^{-\lambda_1 t}, \qquad A_2 = A_1 \frac{\lambda_1}{\lambda_2 - \lambda_1}$$

Transient equilibrium

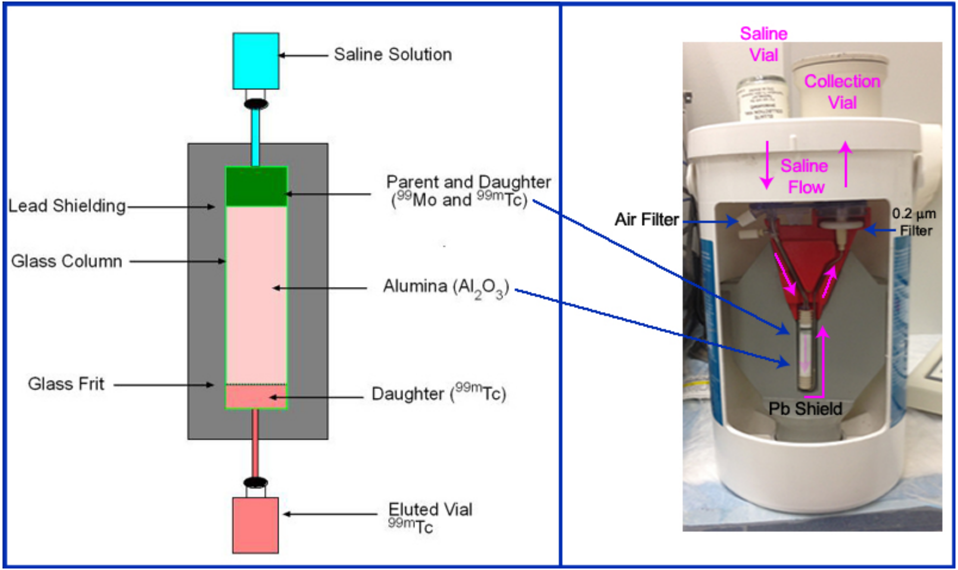


$^{99}_{42}$Mo/$^{99m}_{43}$Tc generator, A_1, A_2

Technetium generator

- ${}^{99}_{42}$Mo produced by fission or neutron bombardment, half-life 67 h
- Adsorbed to alumina Al_2O_3
- ${}^{99}_{42}\text{Mo} \xrightarrow{\beta} {}^{99m}_{43}\text{Tc}$ (and 15% to ${}^{99}_{43}$Tc),
- ${}^{99m}_{43}$Tc half-life 6 h
- ${}^{99m}_{43}$Tc is eluted by physiological saline solution
- ${}^{99m}_{43}$Tc can by chemically manipulated
- When unused, the ratio ${}^{99}_{43}\text{Tc}/{}^{99m}_{43}\text{Tc}$ increases

Technetium generator (2)



Radionuclides produced by generators

Parent P	Parent Half-Life	Mode of Decay P → D	Daughter D	Mode of Decay of D	Daughter Half-Life	Daughter γ Energy (keV)
^{62}Zn	9.1 h	β^+	^{62}Cu	β^+	9.8 min	511
		EC		EC		1173
^{68}Ge	280 days	EC	^{68}Ga	β^+	68 min	511
				EC		1080
^{81}Rb	4.7 h	EC	^{81}Kr^m	IT	13 s	190
^{82}Sr	25 days	EC	^{82}Rb	EC	76 s	777
				β^+		511
^{99}Mo	66.02 h	β^-	^{99}Tc^m	IT	6.02 h	140
^{113}Sn	115.1 days	EC	^{113}In^m	IT	1.66 h	392
^{195}Hg^m	40 h	IT	^{195}Au^m	IT	30.6 s	262
		EC				

Ion bombardment

- Charged particles: mostly $\mathrm{p} = {}^{1}_{1}\mathrm{H}^{+}$, also ${}^{2}_{1}\mathrm{D}^{+}$, ${}^{3}_{2}\mathrm{He}^{2+}$, ${}^{4}_{2}\mathrm{He}^{2+}$
- Accelerated to high energies by a linear accelerator or cyclotron (typical $E_p \sim 18\,\mathrm{MeV}$)
- hit target, get absorbed in the nucleus, knock out a neutron
- Typical reactions

$$
\begin{aligned}
{}^{11}_{5}\mathrm{B} + \mathrm{p} &\longrightarrow {}^{11}_{6}\mathrm{C} + \mathrm{n} \\
{}^{68}_{30}\mathrm{Zn} + \mathrm{p} &\longrightarrow {}^{67}_{31}\mathrm{Ga} + 2\mathrm{n} \\
{}^{18}_{8}\mathrm{O} + \mathrm{p} &\longrightarrow {}^{18}_{9}\mathrm{F} + \mathrm{n}
\end{aligned}
$$

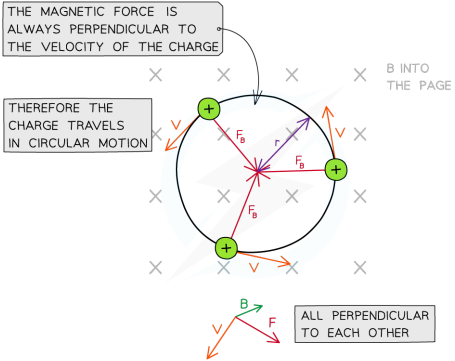
- neutron deficit $\longrightarrow \beta^{+}$ emitters (or EC), mostly short-lived

Radionuclides produced by ion bombardment

Radionuclide	Principal Gamma-Ray Energy (keV)	Half-Life	Production Reaction
^{11}C	511 (β^+)	20.4 min	$^{14}N(p, \alpha)^{11}C$
^{13}N	511 (β^+)	9.96 min	$^{13}C(p, n)^{13}N$
^{15}O	511 (β^+)	2.07 min	$^{15}N(p, n)^{15}O$
^{18}F	511 (β^+)	109.7 min	$^{18}O(p, n)^{18}F$
^{67}Ga	93, 184, 300	78.3 h	$^{68}Zn(p, 2n)^{67}Ga$
^{111}In	171, 245	67.9 h	$^{112}Cd(p, 2n)^{111}In$
^{120}I	511 (β^+)	81 min	$^{127}I(p, 8n)^{120}Xe \rightarrow {}^{120}I$
^{123}I	159	13.2 h	$^{124}Te(p, 2n)^{123}I$ $^{127}I(p, 5n)^{123}Xe \rightarrow {}^{123}I$
^{124}I	511 (β^+)	4.2 days	$^{124}Te(p, n)^{124}I$
^{201}Tl	68–80.3	73 h	$^{203}Tl(p, 3n)^{201}Pb \rightarrow {}^{201}Tl$

Charged particle in a magnetic field

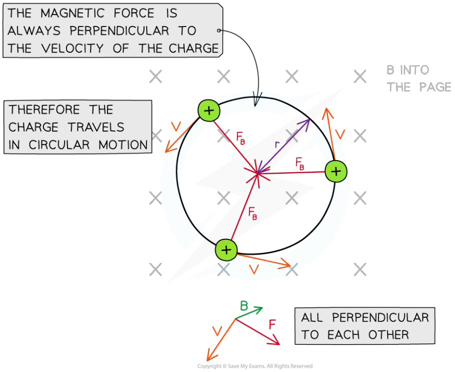
Cyclotron principle



- Magnetic (Lorentz) force $\mathbf{F} = \mathbf{I} \times \mathbf{B} = q\mathbf{v} \times \mathbf{B}$, perpendicular to $\mathbf{v}$ and $\mathbf{B}$ $\longrightarrow$ circular motion

Charged particle in a magnetic field

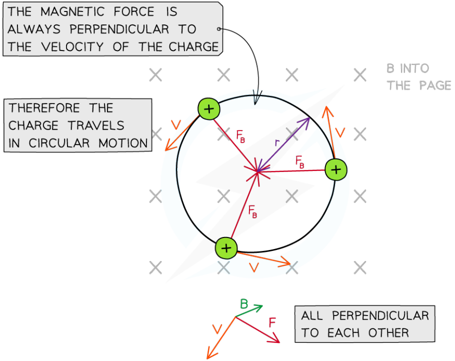
Cyclotron principle



- Magnetic (Lorentz) force $\mathbf{F} = \mathbf{I} \times \mathbf{B} = q\mathbf{v} \times \mathbf{B}$, perpendicular to $\mathbf{v}$ and $\mathbf{B}$ $\longrightarrow$ circular motion
- Centripetal=centrifugal force $F = mv^2/r$

Charged particle in a magnetic field

Cyclotron principle



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- $r = \frac{mv}{Bq}$, since $v \sim r \sim I \longrightarrow$ constant F

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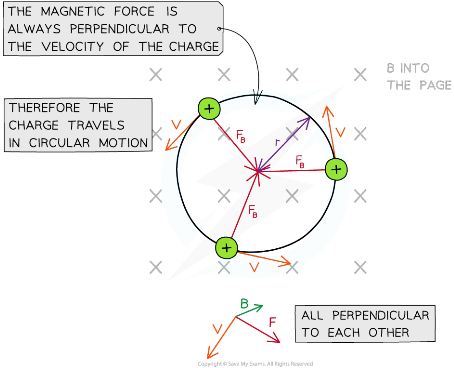
Cyclotron principle



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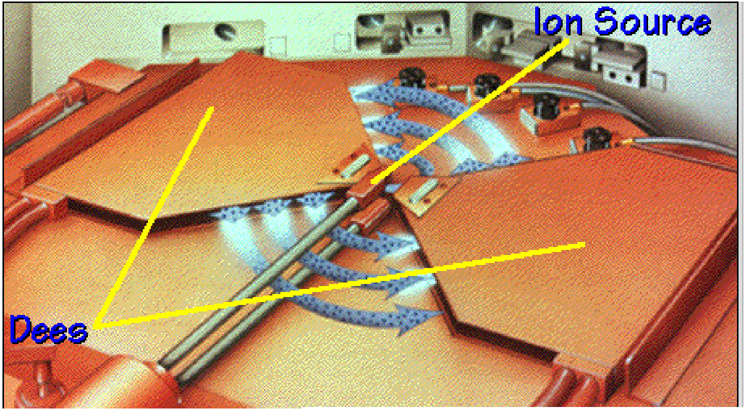
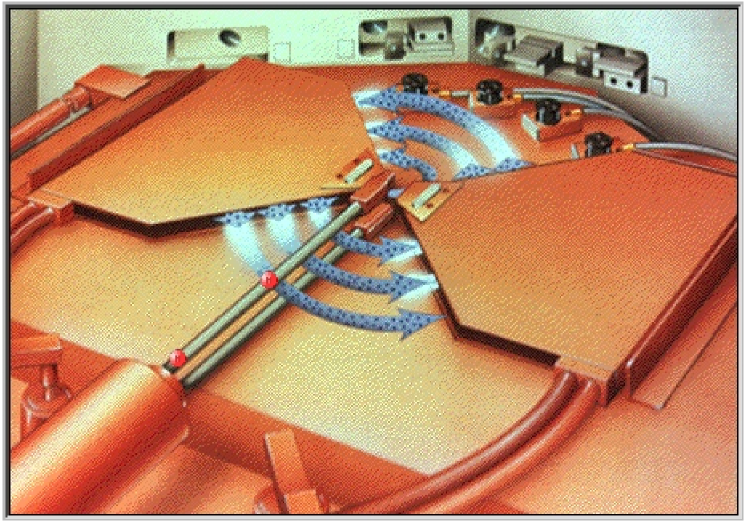
- Neglecting relativistic mass increase, electrode shape

Cyclotron



- Vacuum
- Ion source (batch), mostly H^-
- Hollow 'D' electrodes, high frequency AC voltage (MHz)
- Magnetic field (oriented vertically)

Cyclotron



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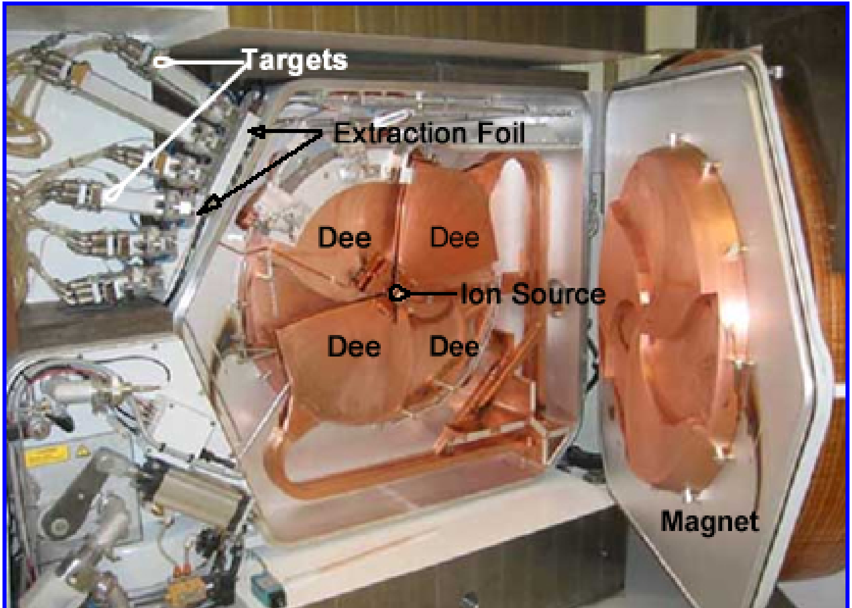
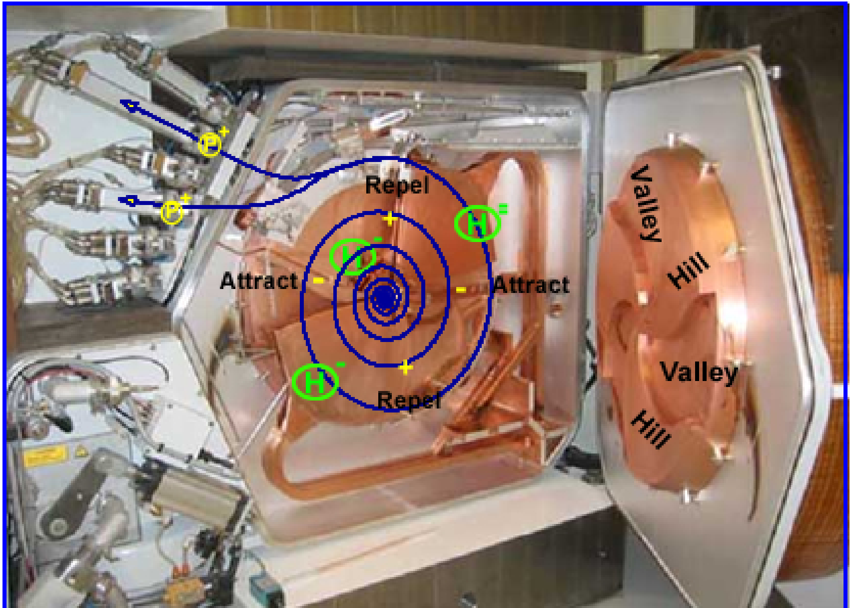
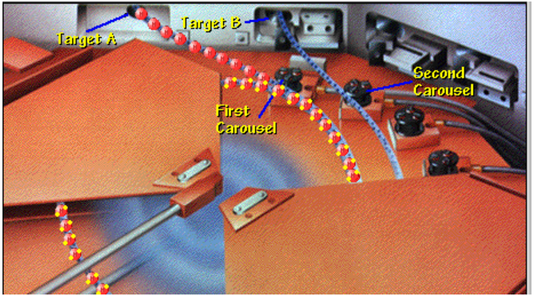
Real cyclotron



Real cyclotron

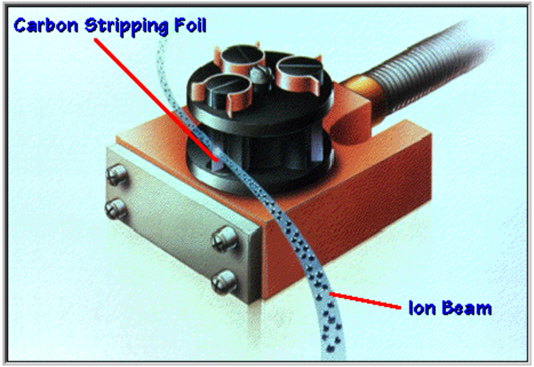


Carousel



- after $\sim$ 100s of cycles
- H^- ion hits a thin carbon foil
- $\longrightarrow$ looses electrons, converted $p = H^+$
- $\longrightarrow$ opposite curvature
- Only part of the beam is deviated
- Foil lasts $\sim$ 100 hours

Carousel



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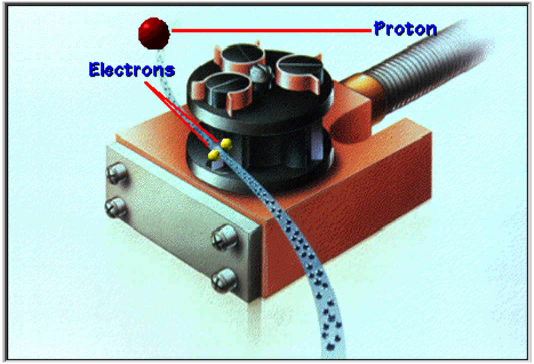

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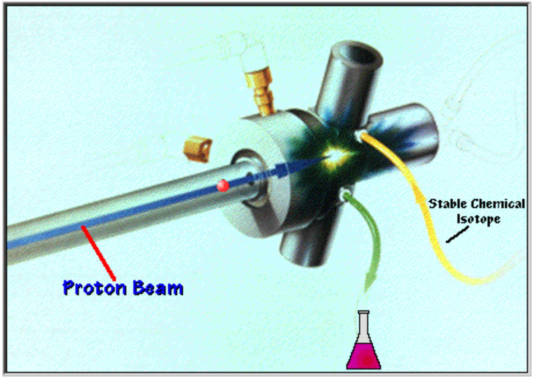
Target chamber

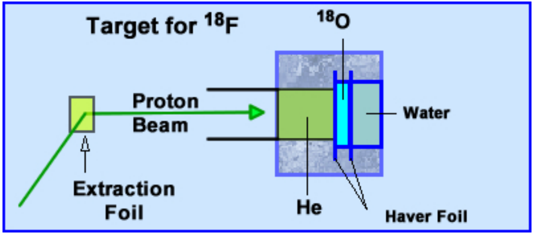
Reakční komora



- Filled with a stable isotope
- Radioactive isotope is created
- Shielded, small, easy to change

Target chamber

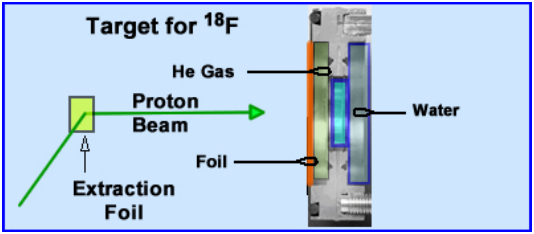
Reakční komora



- $^{18}_{8}$O — rare (0.2%), enrichment needed (distillation, very small ΔT_{boil})
- Cooling needed (by water)
- Thin cobalt alloy foils (havar)
- Every few hours, $^{18}_{9}$F can be extracted

Target chamber

Reakční komora



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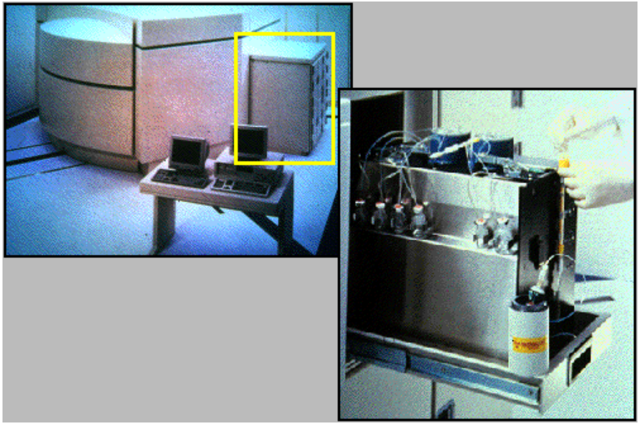
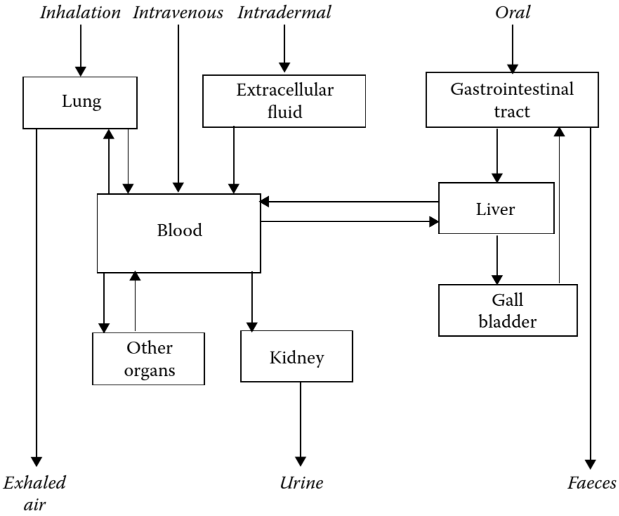
Biosynthesizer



- Radiopharmaceutical — radioactively labeled biologically active/compatible chemical compound.
- Quantitative & qualitative imaging of physiological processes.

Administration, distribution and excretion



Must traverse membranes to get to the targete organ.

Administration of radiopharmaceuticals

- Mostly physiological (saline) solution
- Blood-brain barrier
  - Intravenously administered contrast agent does not get to the brain
  - Contrast agent administered to the cerebro-spinal fluid only gets to the brain and spine.

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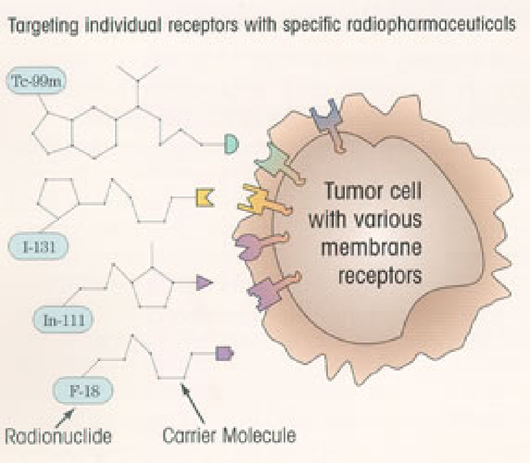
- Imaging afinity and metabolism speed

Radiopharmaceutical construction

Radionuclide + carrier molecule (+ probe)



Radiopharmaceuticals (tracers) for SPECT imaging

Radionuclide	Pharmaceutical	Indication/Use	Typical Administered Activity (MBq)
^{67}Ga	Citrate	Tumour imaging, infection/ inflammation imaging	150[a]
$^{81}Kr^m$	Krypton gas	Lung ventilation imaging	6000[a]
$^{99}Tc^m$	Albumin	Cardiac blood-pool imaging, peripheral vascular imaging	800[a]
$^{99}Tc^m$	Colloids, including tin colloid and sulphur colloid	Oesophageal transit and reflux	40[a]
		Liver imaging	80[a], 200 (SPECT)[a]
		Bone marrow imaging, GI bleeding	400[a]
$^{99}Tc^m$	DTPA	Lung ventilation imaging (aerosol)	80[a]
		Renal imaging/renography	300[a]
		Brain imaging (static)	500[a], 800 (SPECT)[a]
		First-pass blood-flow studies	800[a]
$^{99}Tc^m$	DMSA	Renal imaging (DMSA(III))	80[a]
		Tumour imaging (DMSA(V))	400[a]
$^{99}Tc^m$	ECD	Brain imaging	500[a]
$^{99}Tc^m$	Erythrocytes (normal)	GI bleeding	400[a]
		Cardiac blood-pool imaging or peripheral vascular imaging	800[a]
$^{99}Tc^m$	Erythrocytes (heat denatured)	Spleen imaging	100[a]
$^{99}Tc^m$	Exametazime	Cerebral blood-flow imaging (SPECT)	500[a]
$^{99}Tc^m$	Iminodiacetates (IDAs)	Functional biliary system imaging	150[a]
$^{99}Tc^m$	Leucocytes	Infection/inflammation imaging	200[a]

Radiopharmaceuticals (tracers) for SPECT imaging

Radionuclide	Pharmaceutical	Indication/Use	Typical Administered Activity (MBq)
$^{99}Tc^{m}$	Macroaggregated albumin	Lung perfusion imaging	100[a], 200 (SPECT)[a]
$^{99}Tc^{m}$	MAG3	Renal imaging/renography	100[a]
		First-pass blood-flow imaging	200[a]
$^{99}Tc^{m}$	Nanocolloids	Lacrimal drainage	4[a]
		Sentinel node or lymph node imaging	20[a]
$^{99}Tc^{m}$	Pertechnetate	Micturating cystogram	25[a]
		Thyroid uptake	40[a]
		Thyroid imaging, salivary gland imaging	80[a]
		Ectopic gastric mucosa imaging (Meckel's)	400[a]
		First-pass blood-flow imaging	800[a]
$^{99}Tc^{m}$	Phosphonate and phosphate compounds	Bone imaging	600[a], 800 (SPECT)[a]
$^{99}Tc^{m}$	Sestamibi	Myocardial imaging	300[a], 400 (SPECT)[a]
		Tumour imaging, breast imaging	900[a]
$^{99}Tc^{m}$	Sulesomab	Infection/inflammation imaging	750[a]
$^{99}Tc^{m}$	Technegas	Lung ventilation imaging	40[a]
$^{99}Tc^{m}$	Tetrofosmin	Myocardial imaging	300[a], 400 (SPECT)[a]
		Parathyroid imaging	900[a]
^{111}In	Capromab Pendetide	Biopsy-proven prostate carcinoma imaging	185[b]
^{111}In	DTPA	GI transit	10[a]
		Cisternography	30[a]

Radiopharmaceuticals (tracers) for SPECT imaging

Radionuclide	Pharmaceutical	Indication/Use	Typical Administered Activity (MBq)
^{111}In	Leucocytes	Infection/inflammation imaging	20[a]
^{111}In	Pentetreotide	Somatostatin receptor imaging	110[a], 220 (SPECT)[a]
^{111}In	Platelets	Thrombus imaging	20[a]
^{123}I	Iodide	Thyroid uptake	2[a]
		Thyroid imaging	20[a]
		Thyroid metastases imaging	400[a]
^{123}I	Ioflupane	Striatal dopamine transporter visualisation	185[a]
^{123}I	*m*IBG	Neuroectodermal tumour imaging	400[a]
^{131}I	*m*IBG	Neuroectodermal tumour imaging	20[a]
^{131}I	Iodide	Thyroid uptake	0.2[a]
		Thyroid metastases imaging	400[a]
^{133}Xe	Xenon gas	Lung ventilation studies	400[a]
^{201}Tl	Thallous chloride	Myocardial imaging	80–120[a]
		Parathyroid imaging	80[a]
		Tumour imaging	150[a]

Radiopharmaceuticals (tracers) for SPECT imaging

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^{111}In	Leucocytes	Infection/inflammation imaging	20[a]
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^{123}I	Iodide	Thyroid uptake	2[a]
		Thyroid imaging	20[a]
		Thyroid metastases imaging	400[a]
^{123}I	Ioflupane	Striatal dopamine transporter visualisation	185[a]
^{123}I	*m*IBG	Neuroectodermal tumour imaging	400[a]
^{131}I	*m*IBG	Neuroectodermal tumour imaging	20[a]
^{131}I	Iodide	Thyroid uptake	0.2[a]
		Thyroid metastases imaging	400[a]
^{133}Xe	Xenon gas	Lung ventilation studies	400[a]
^{201}Tl	Thallous chloride	Myocardial imaging	80–120[a]
		Parathyroid imaging	80[a]
		Tumour imaging	150[a]

and others: selenium ^{75}Se...

Pharmaceuticals for PET imaging

Oxygen ^{15}O

- Half-life ^{15}O is 2.5 min.
- **Carbon dioxide** (CO_2) — brain blood flow
- **Oxygen** (O_2) — oxygen consumption in myocardium, tumors
- **Water** (H_2O) — myocardium perfusion
  - \+ not influenced by metabolism
  - − background ^{15}O activity in lungs and blood vessels

Nitrogen $^{13}\mathrm{N}$

- Half-life $^{13}\mathrm{N}$ is 10 min.
- **Ammonia** $(\mathrm{NH_3})$ — myocardium perfusion, blood flow
  - metabolized in v tissue

Carbon $^{11}\mathrm{C}$

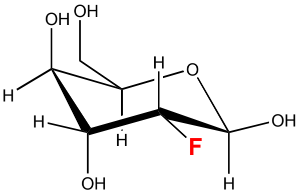
- Half-life $^{11}\mathrm{C}$ is 20.4 min.
- **Acetic acid (CH_3COOH)** — myocardium perfusion, tumor metabolism
- **Cocain, carfentanil,. . .** — brain opiod receptor mechanisms
- **Deprenyl** — monoamine oxidase inhibitor, to study Parkinson disease
- **Leucin, methionine. . .** — amino acid tracer, brain tumor detection
- . . .

Fluorine $^{18}\mathrm{F}$

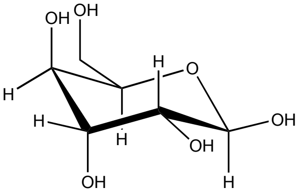
- Half-time $^{18}\mathrm{F}$ is 109 min.
- **Haloperidol** — neuroreceptor ligand, drug effects
- **Sodium fluoride Na**$^{18}\mathrm{F}^{-}$ — skeletal imaging, osseous blood-flow, metastases. Better signal than $^{99m}\mathrm{Tc}$
- **Fluorodopa. . .** — metabolised to dopamine, neurotransmiter studies
- **Flourouracil. . .** — drug, nucleic acid tracer, chemotherapy dosage
- **Fluorodeoxyglucose (FDG)** — glucose metabolism ; neurology, cardiology, oncology. Penetrates blood-brain barier

Delivery Strategies: Metabolic pathways

FDG
2-fluoro-2-deoxy-glucose



B-D-glucose



FDG usage

- Brain function mapping
- . . . *glucose* provides energy to the brain (for adults $\sim 100\,\text{g/den}$)

FDG usage

- Brain function mapping
- . . . *glucose* provides energy to the brain (for adults $\sim 100\,\mathrm{g/den}$)
- Tumor mapping
- . . . tumors have no metabolic barier

FDG in Oncology

- FDG transport into tumors occurs at a *higher* rate than in the surrounding normal tissues.
- FDG is de-phosphorylated and can then leave the cell.
- The dephosphorylation occurs at a *slower* rate in tumors.

Applications of FDG

- Locating unknown primaries
- Differentiation of tumor from normal tissue
- Pre-operative staging of disease (lung, breast, colorectal, melanoma, H&N, pancreas)
- Recurrence vs necrosis
- Recurrence vs post-operative changes (limitations with FDG)
- Monitoring response to therapy

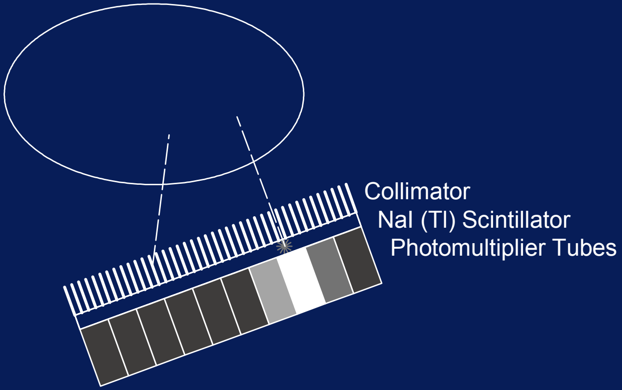
Rubidium $^{82}\mathrm{Rb}$

- Half-life $^{82}\mathrm{Rb}$ is 1.25 min.
- \+ Produced by a generator from Sr, (no cyclotron needed)
- – Long positron free path $\longrightarrow$ low spatial spatial resolution.
- \+ Short half-life $\longrightarrow$ good temporal resolution
- – Short half-life $\longrightarrow$ weak signal
- Myocard perfusion
- Blood-brain barrier study

Gamma camera

Scintigraphy

Single Photon Detection with Gamma Camera

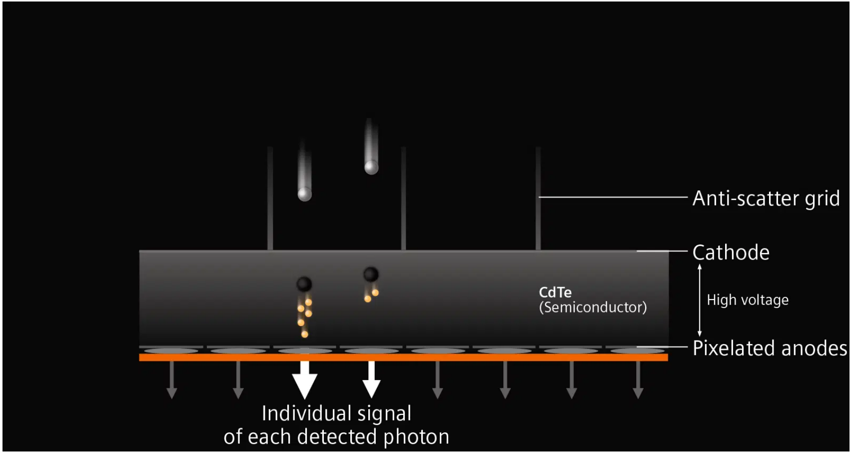


Scintillator materials

Scintillator	Density (g cm^{-3})	Effective Z	Relative light yield	Decay constant (ns)	Wavelength of emission (nm)
Sodium Iodide (NaI)	3.67	50	100	230	410
Bismuth Germanate (BGO)	7.13	74	12	300	480
Barium Fluoride (BaF_2)	4.89	54	5 15	0.6 - 0.8 630	220 (195) 310

- High Z advantageous
- BGO good for 511 keV
- For speed, use $\mathrm{BaF_2}$ — UV light produced

Photon Counting Detector (PCD)

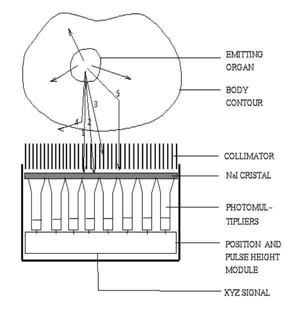


- Signal propagation directed by electric field
- High quantum efficiency
- High spacial resolution

Artifacts: scattering

Scattering of photons in patient

- Because of limited energy resolution of the detector, primary and scattered photons which pass the collimator can not be classified properly. (In the ideal case, only primary photons are used to contribute to the image)
- Effects: haziness of images, quantization is degraded.



Artifacts: collimator blur

Collimator blur

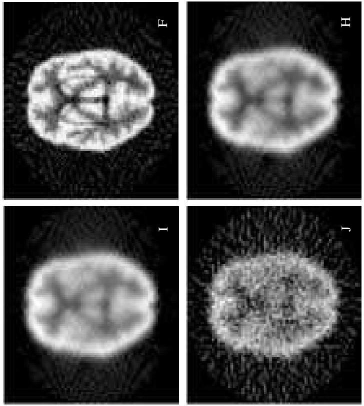
- Because of the size of the holes, photons which are not entering the detector exactly perpendicular to the detector surface are also detected. This introduces uncertainty about the exact path the photon traveled.
- Effect: blurring which increases with larger holes. Trade off between sensitivity and resolution has to be found.

Artifacts: noise

Noise due to limited number of detected photons

- Doses and scanning time are limited while the efficiency of the collimator is also limited.
- Effects: Noise in the images. Low pass digital filtering required. This results in reduced resolution. Tradeoffs between dose, scanning time and collimator hole size have to be made.

Phantom experiments



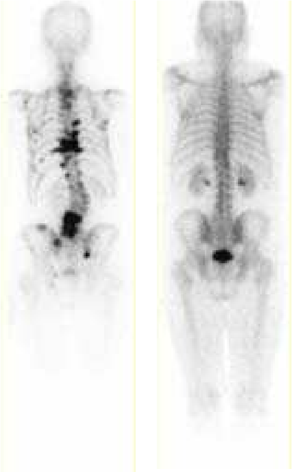
Ground truth phantom

Detector + attenuation

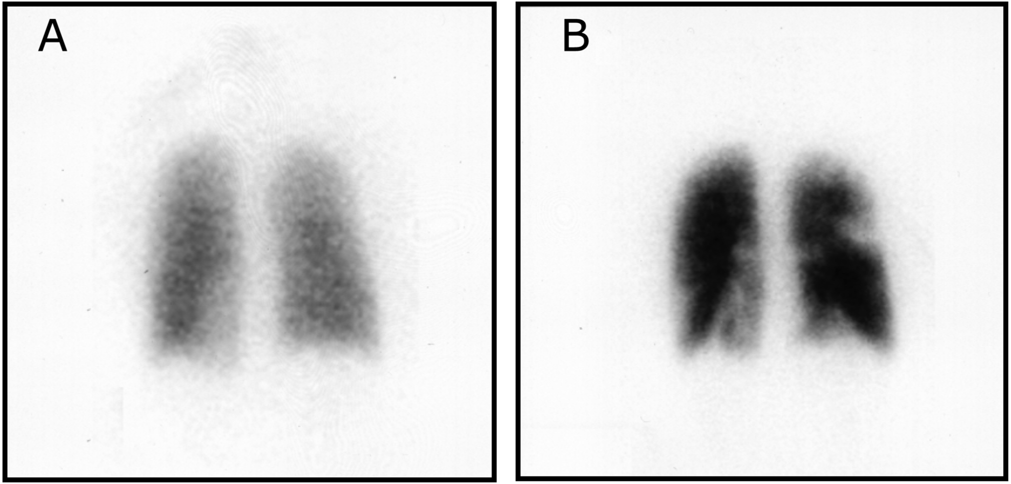
Detector + attenuation + scatter

Detector + attenuation + scatter + noise

Scintigram



Lung scintigraphy



Most frequent use.

Ventilation (Xe), perfusion (^{99m}Tc). Pulmonary embolism (blocked artery)

Principles of nuclear imaging

Radioactivity

Gamma camera

SPECT

PET

Conclusions

SPECT

Single Photon Emission Computed Tomography (SPECT)

Image is acquired by rotating the γ-camera around the patient and taking images at different angles

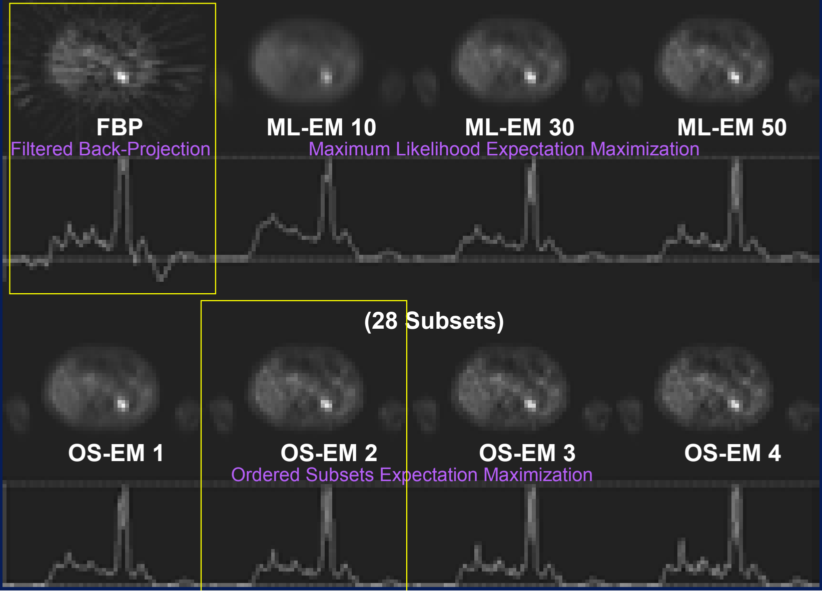
SPECT

- Patient is injected with a γ-emitting radio-pharmaceutical
- Preferred energy: 100-250 keV
- Use of collimaters
- Collimated camera projections are acquired from different equidistant angles (30-120 projections over 180-360 degrees)
- Images are reconstructed using Filtered Back Projection (FBP) or Iterative Reconstruction
- Resolution: 12-20 mm
- To increase count-rate often two or three γ-camera heads are used

SPECT

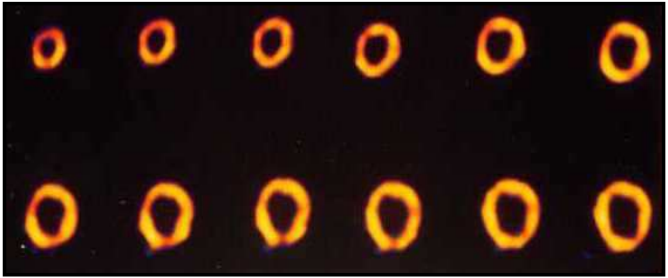
SPECT, brain imaging

Image Reconstruction Methods

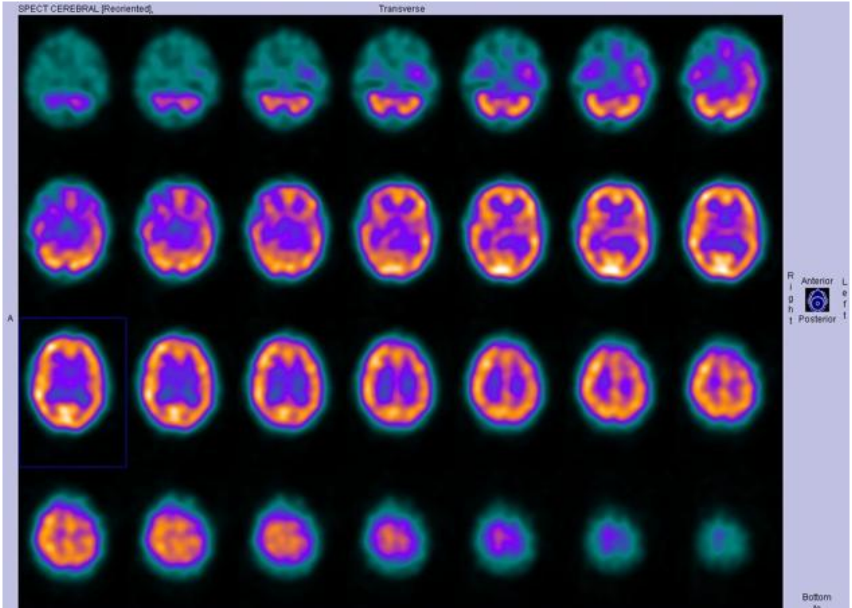


SPECT: Applications

Cardiac Imaging

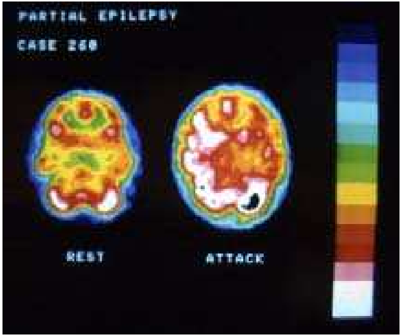


SPECT, Brain perfusion

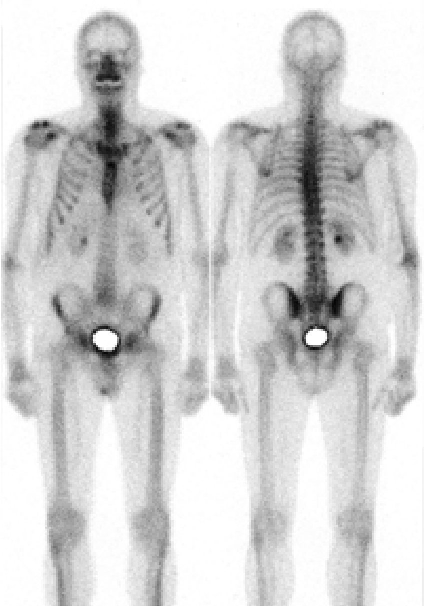


SPECT: Applications

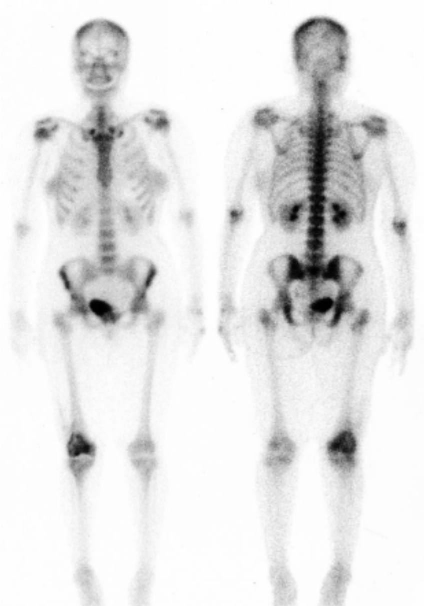
Epilepsy



SPECT, Whole-body imaging



SPECT, Whole-body imaging



Principles of nuclear imaging

Radioactivity

Gamma camera

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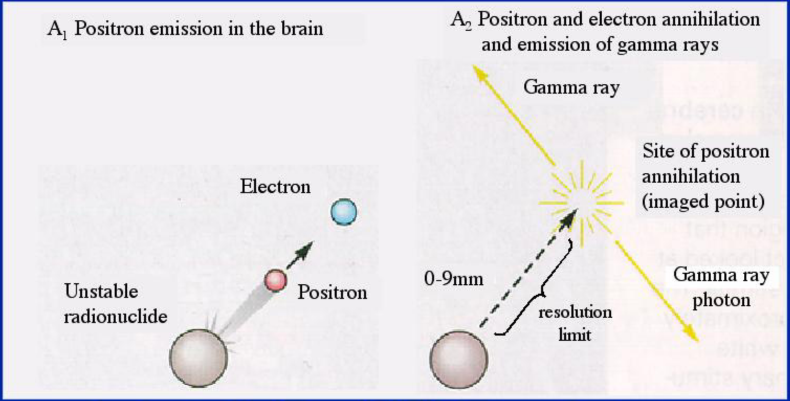
PET

Conclusions

Principle of PET

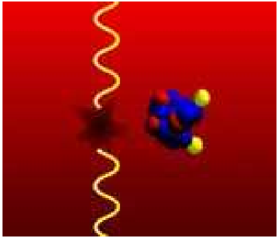


From: Principles of Neural Science (4th. Ed.) Kandel, Schwartz, & Jessell, p. 377.

Columbia fMRI

PET: annihilation

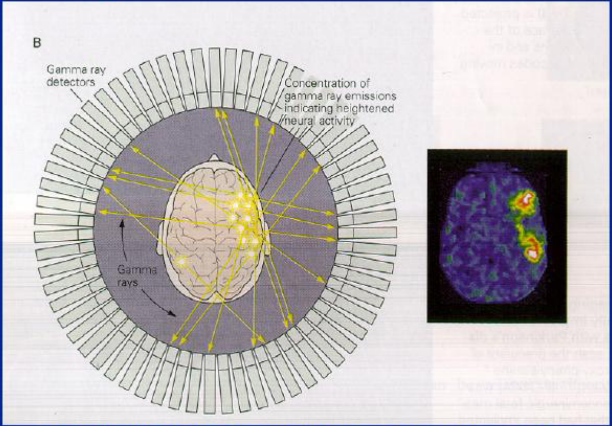
$$p \rightarrow n + \beta^{+}$$



Annihilation
Coincidence
Detection

Isotope	Maximum Positron Range (mm)
F-18	2.6
C-11	3.8
Ga-68	9.0
Rb-82	16.5

Gamma Ray Detections to Location of Function



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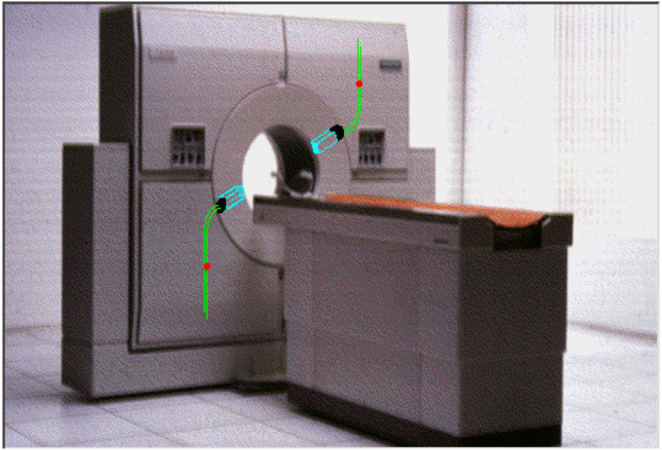
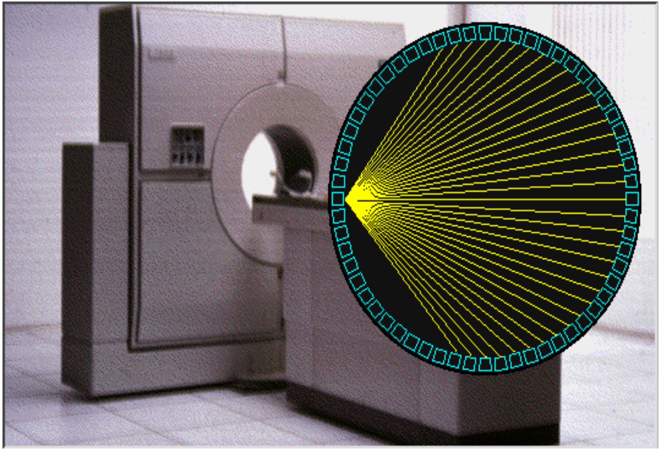
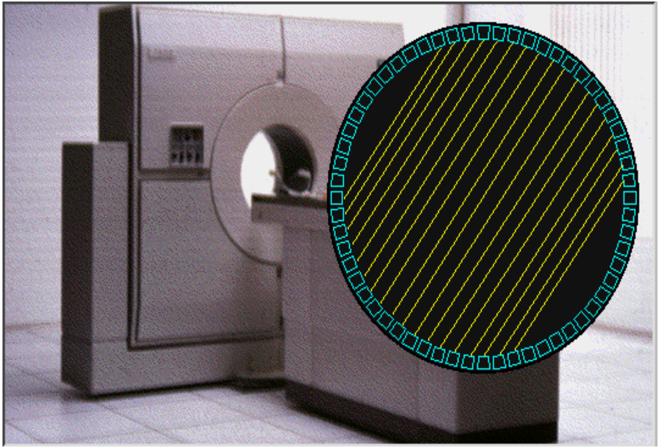
PET



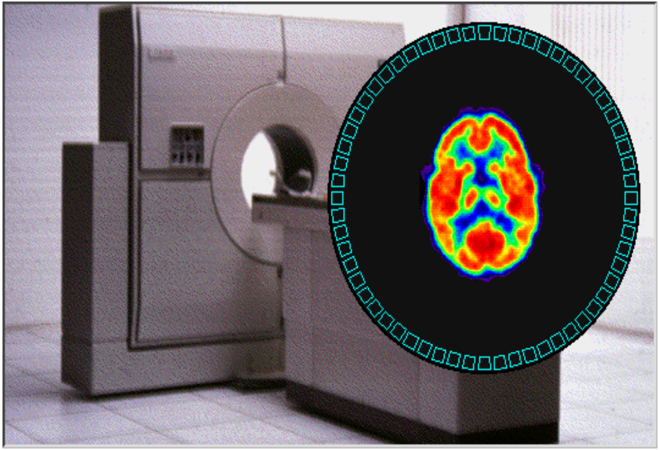
PET



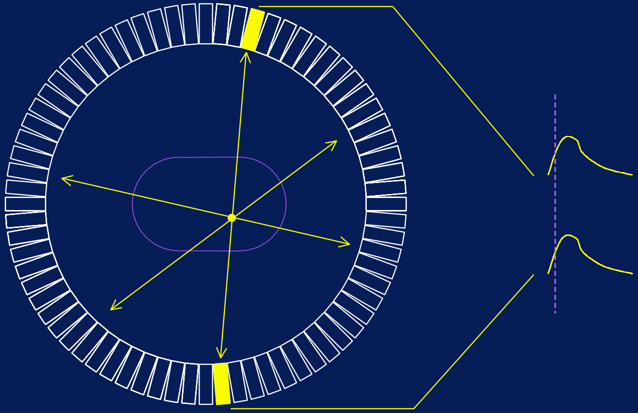
PET



PET



Coincidence Event

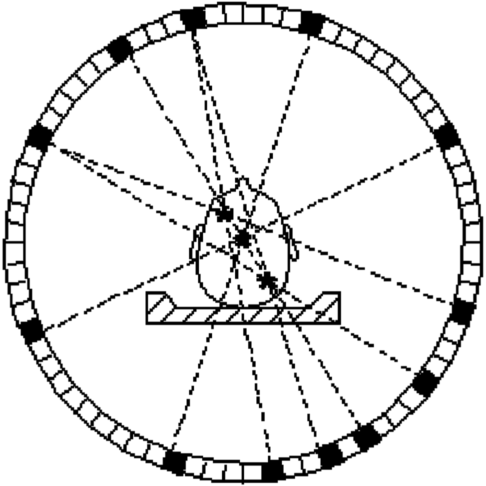


Electronic collimation

- Associate detections within interval τ (a few ns)
- Start timer and wait for the second detection $\longrightarrow$ increment count
- *List mode* — store detections with time stamps, postprocess
- No lead collimators $\longrightarrow$ higher sensitivity wrt SPECT

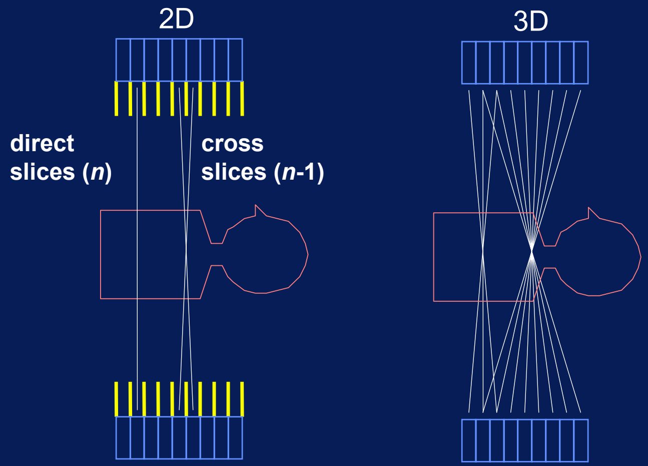
Time of Flight PET

- Measure time interval between coincident photones



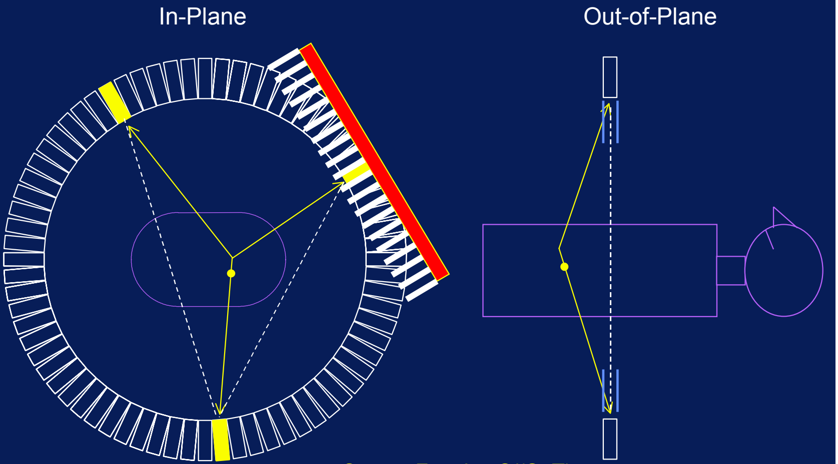
Multiple Rings, 2D – 3D

For *n* detector rings:



total slices = 2*n*-1

Scattered Coincidence Event

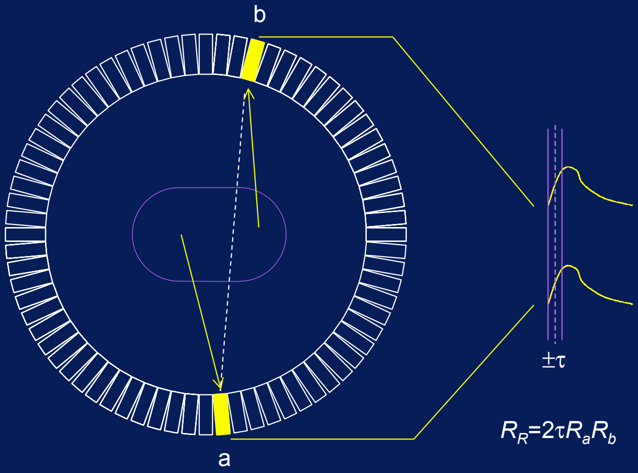


<u>Scatter Fraction S/(S+T)</u>

With septa ~10-20%

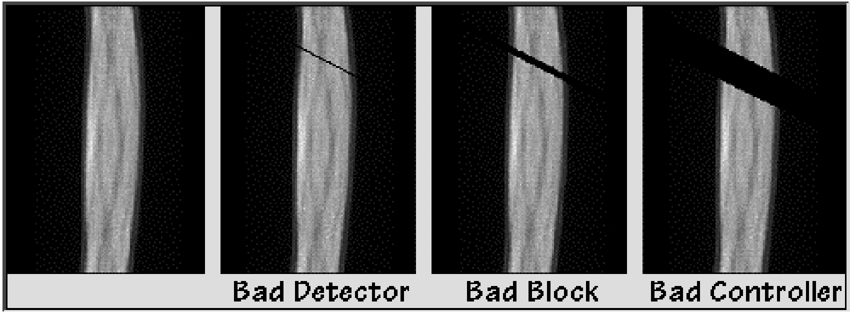
w/o septa ~30-80%

Random Coincidence Event



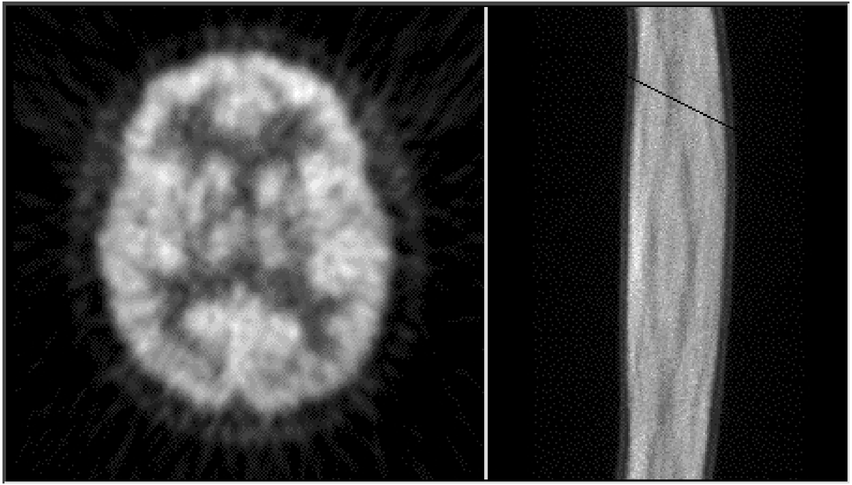
$R_R = 2\tau R_a R_b$

Detector failure



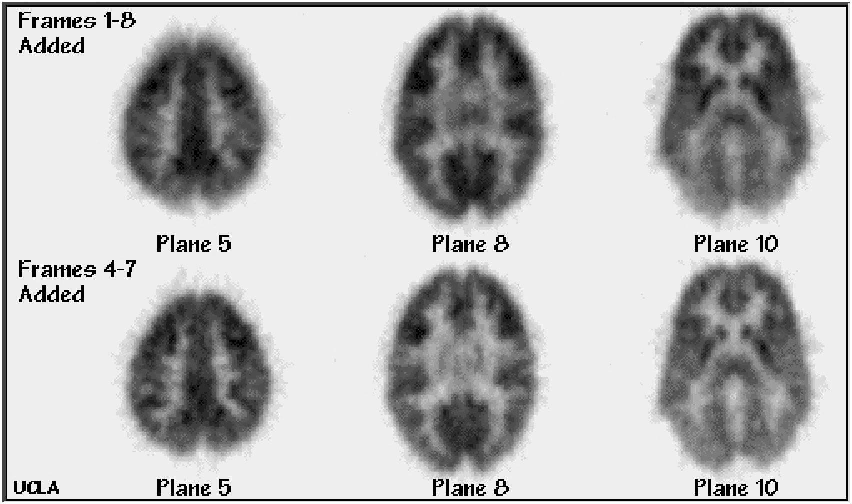
Sinogram

Detector failure



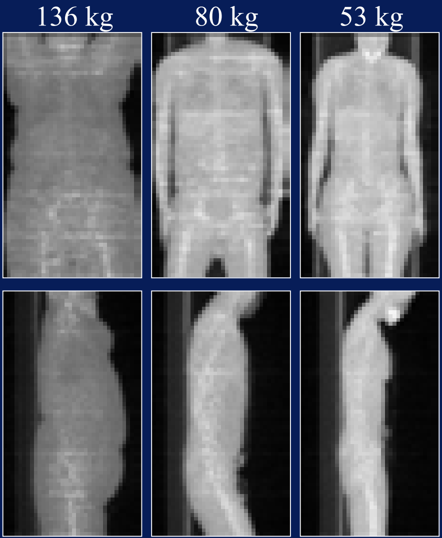
Rekonstrukce

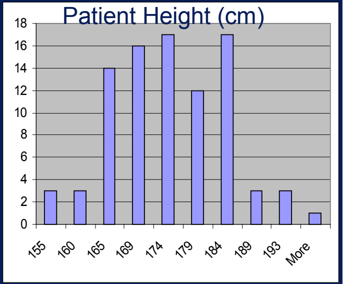
Patient motion

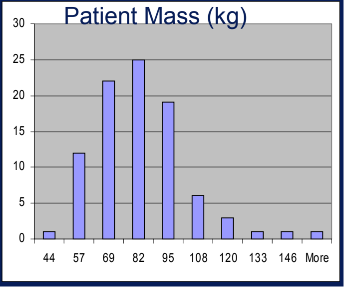


Lower row only uses images without motion.

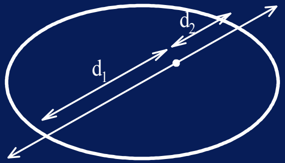
Patient Size Variations







Coincidence Attenuation



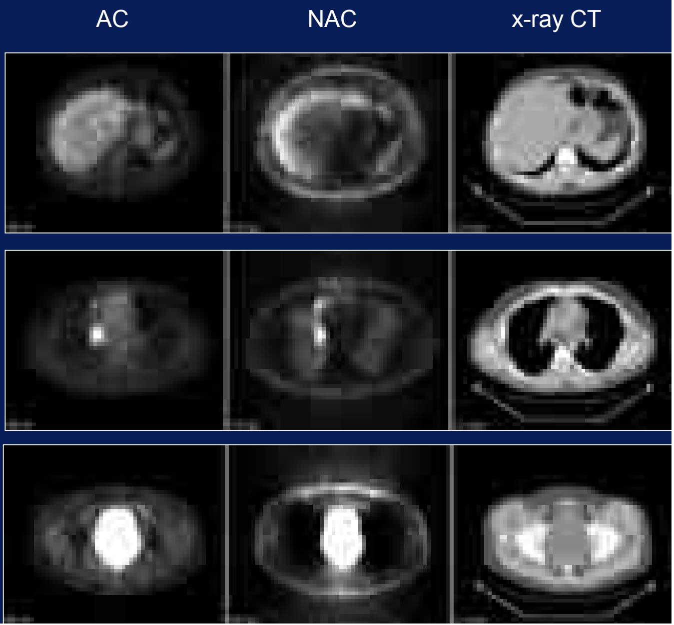
$$P_C = P_1 P_2$$

$$= e^{-\mu \cdot d_1} e^{-\mu \cdot d_2}$$

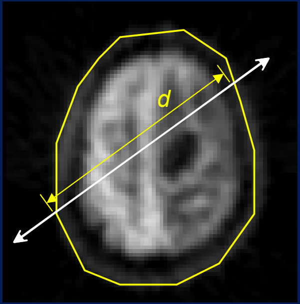
$$= e^{-\mu \cdot (d_1 + d_2)}$$

Annihilation radiation emitted along a particular line of response has the same attenuation probability, regardless of where it originated on the line.

Attenuation Effects

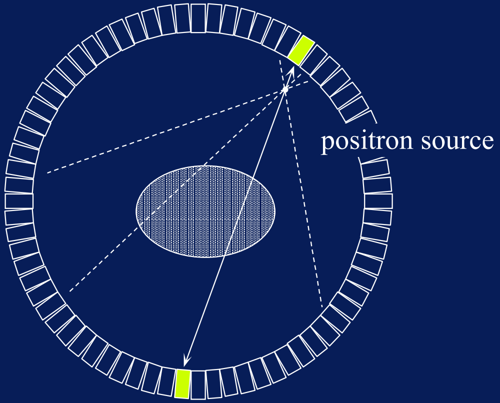


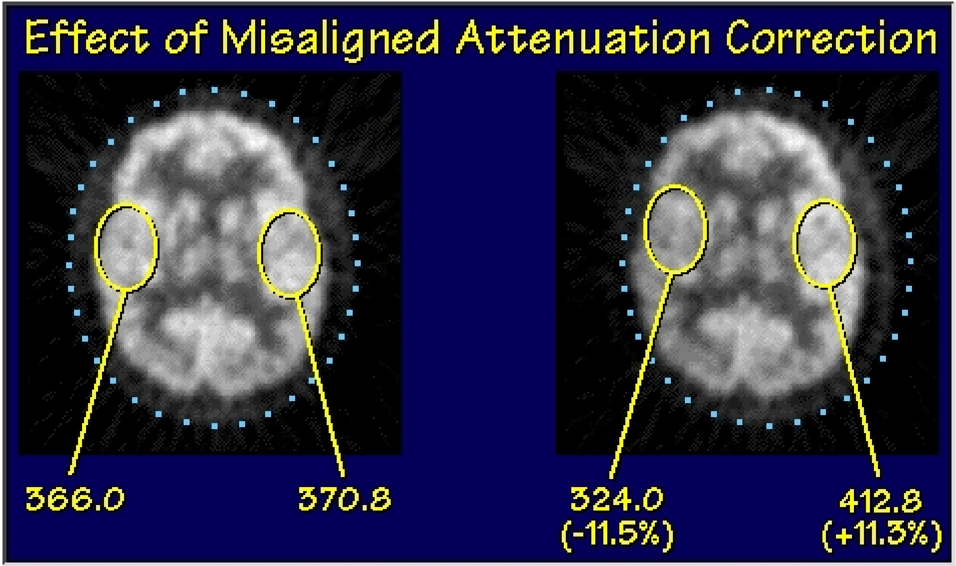
Calculated Attenuation Correction

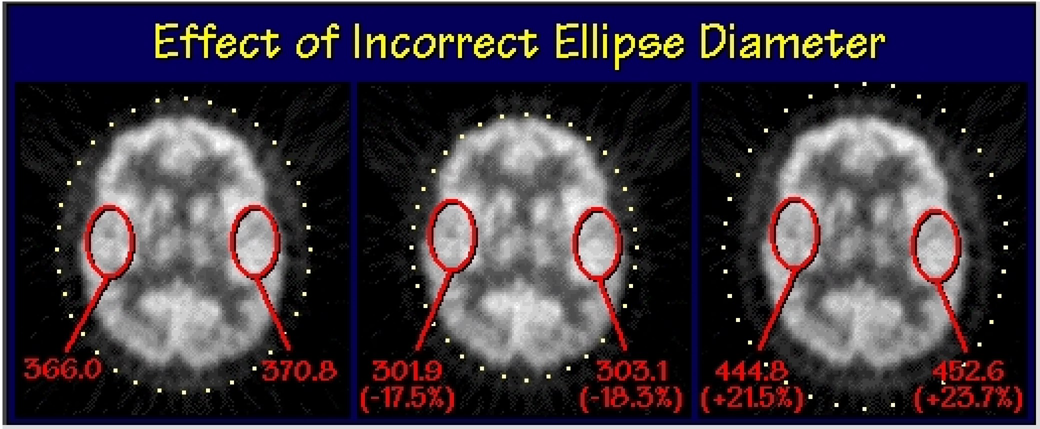


$$I = I_0 e^{-\mu d}$$

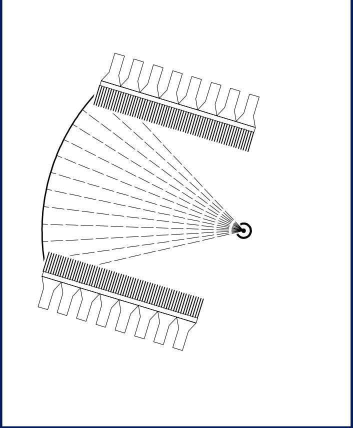
Transmission Attenuation Measurement



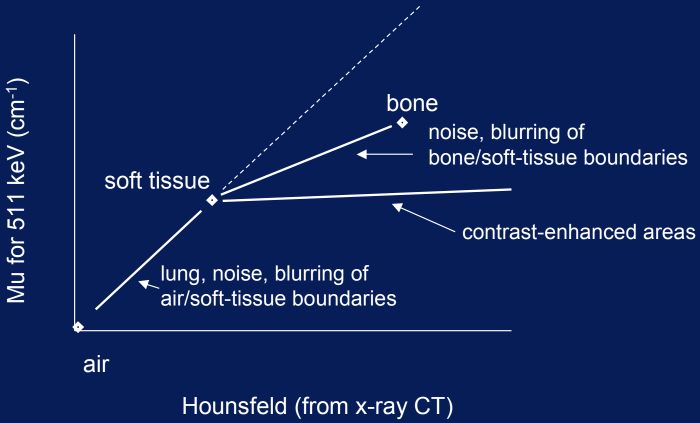

Effect of Misaligned Attenuation Correction
366.0
370.8
324.0
(-11.5%)
412.8
(+11.3%)


Effect of Incorrect Ellipse Diameter
366.0
370.8
301.9
(-17.5%)
303.1
(-18.3%)
444.8
(+21.5%)
452.6
(+23.7%)

SPECT/CT



Converting Attenuation Map from Hounsfeld to 511 keV attenuation Coefficients

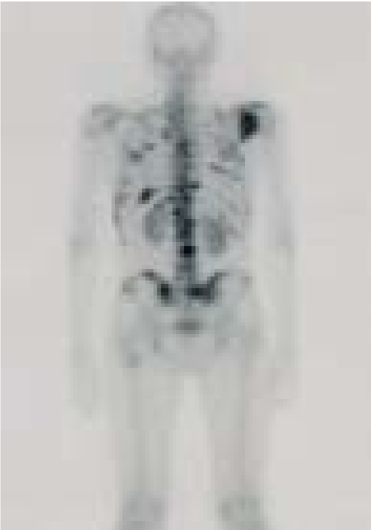


PET — parametry

- Effective resolution $8 \sim 10\,\mathrm{mm}$
- Isotropic sampling $3\,\mathrm{mm}$
- Transaxial FOV $60\,\mathrm{cm}$, axial $10\,\mathrm{cm}$. Increase axial FOV by increasing number of detectors (=higher cost), or shift the patient (=longer time, higher dose).
- $16 \sim 64$ detector planes zachování linearity.

PET, whole body imaging

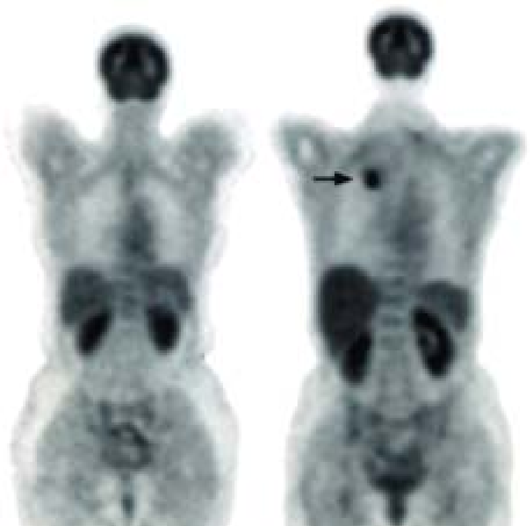
Tumor has faster metabolism $\longrightarrow$
contrast agents accumulates there



PET + FDG

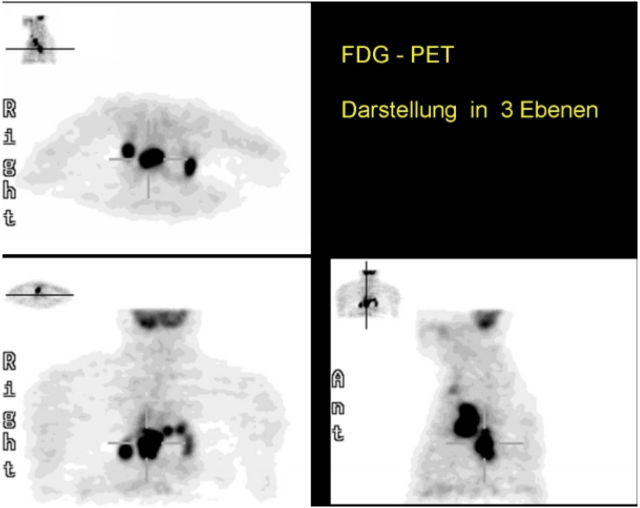
^{18}F glucose (FDG)

Normal Lung tumor



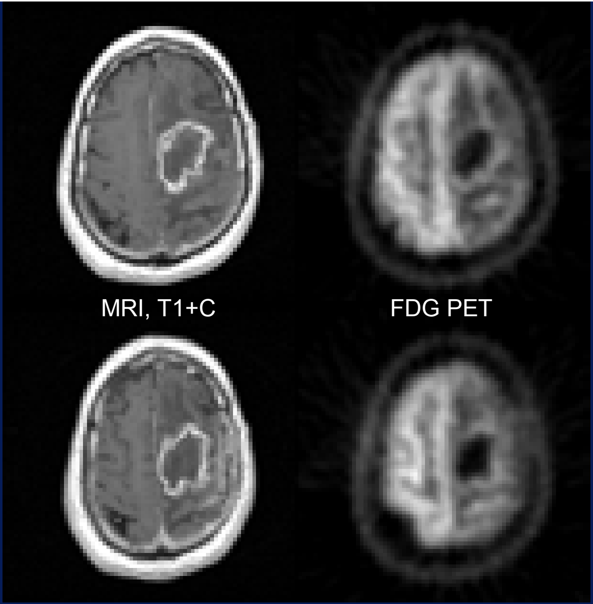
PET + FDG

^{18}F glucose (FDG). Tumor detection.

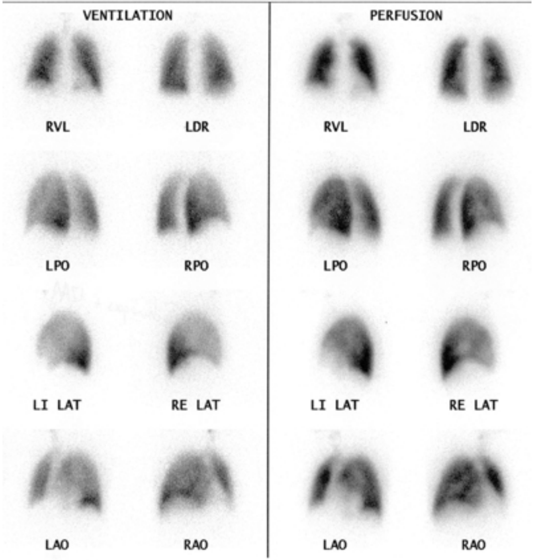


Brain Tumor
FDG

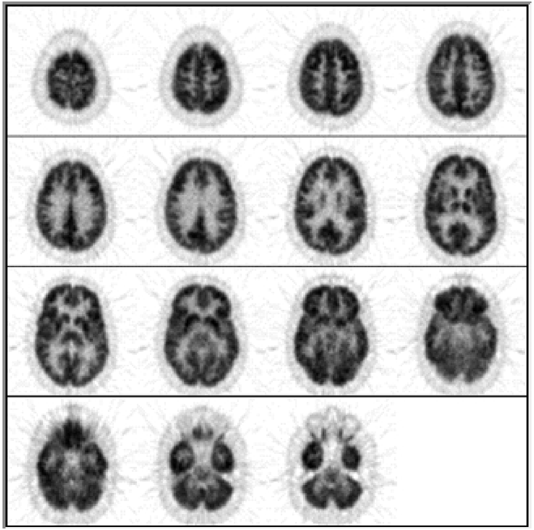
6 min, 3D



PET. Lung ventilation and perfusion



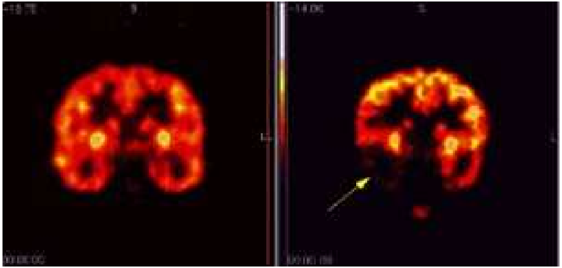
PET, head



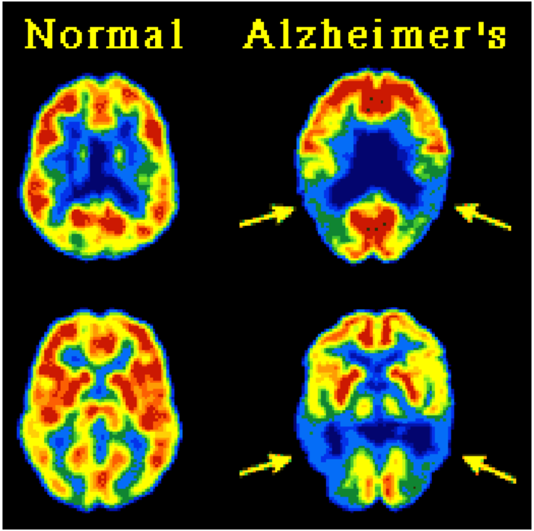
perfusion, glucose metabolism

PET: Applications

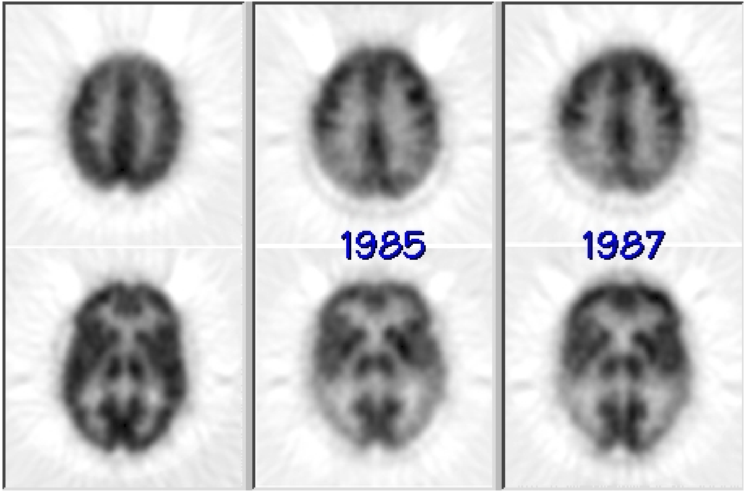
Brain imaging



PET, brain



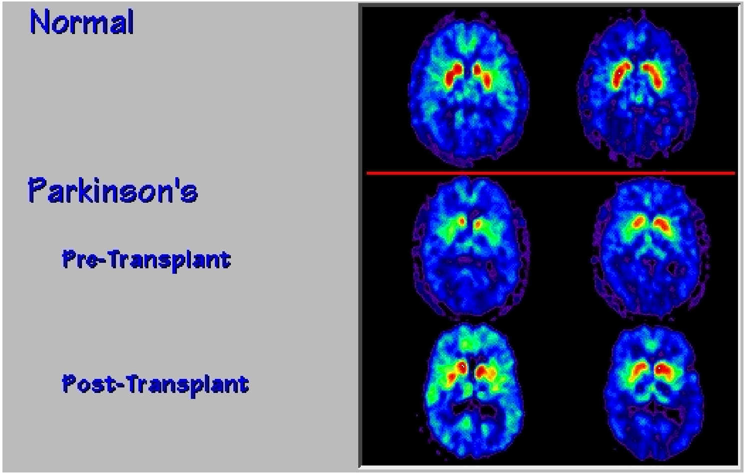
Alzheimer disease



Hypometabolismus.

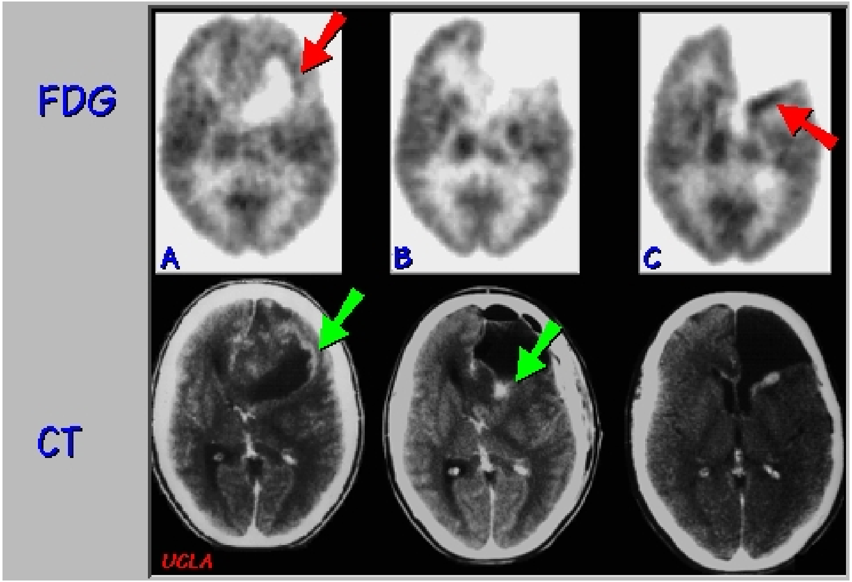
Parkinson disease

$^{18}\mathrm{F-DOPA}$ PET (precursor of neurotransmiter dopamine)



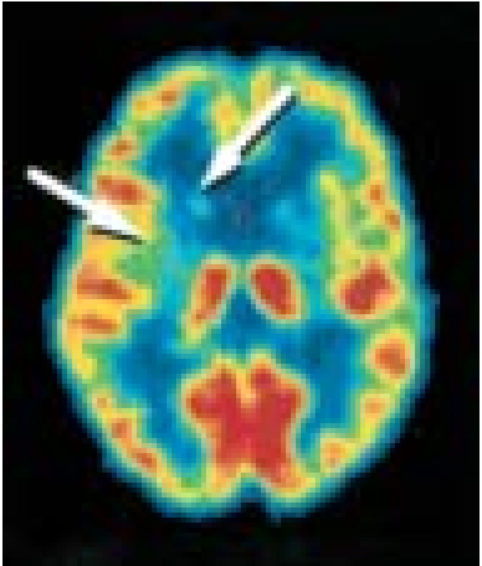
Transplantation of dopamin producing cells.

Brain tumor



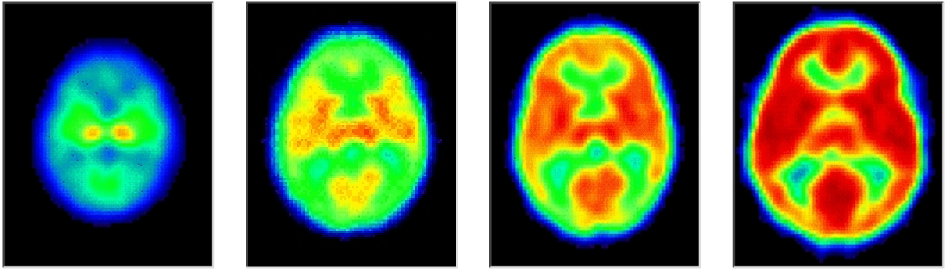
PET, Huntington disease

Reduced glucose metabolism



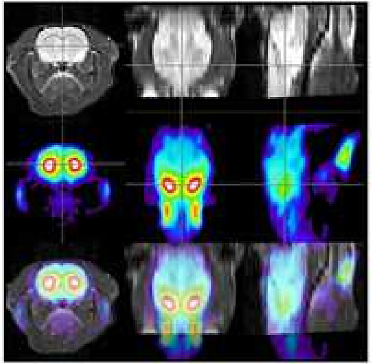
Brain development

FDG



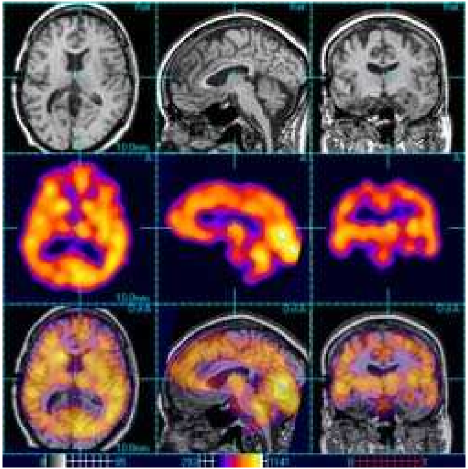
1 month 3 months 6 months 1 year

Fusion of anatomical and functional data

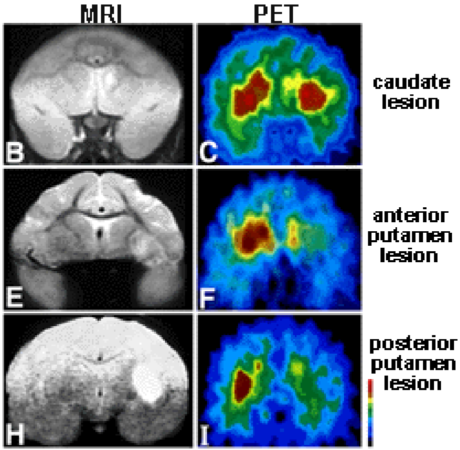


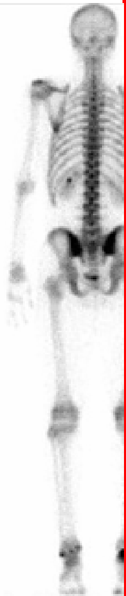
Fusion of anatomical and functional data

Fusion
MRI & SPECT



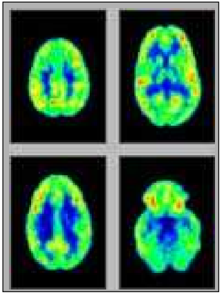
Fusion of anatomical and functional data



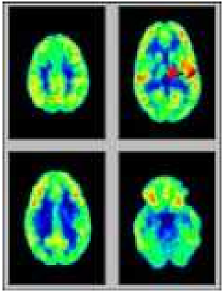


PET: Applications

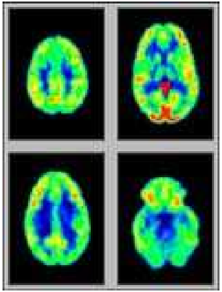
Functional imaging



rest

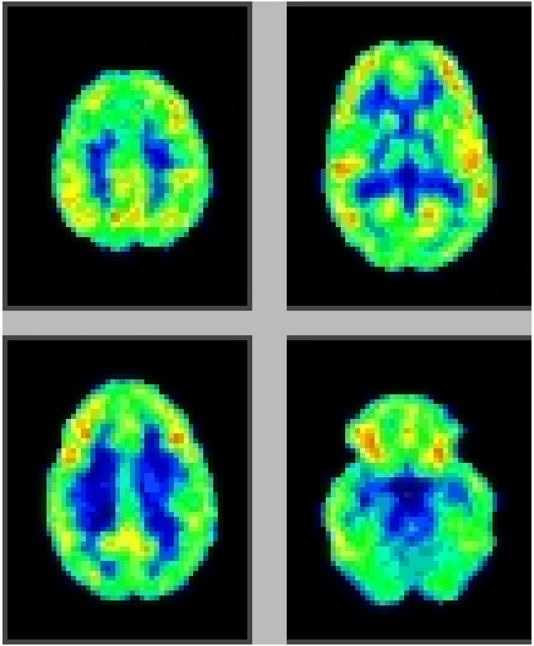


hear

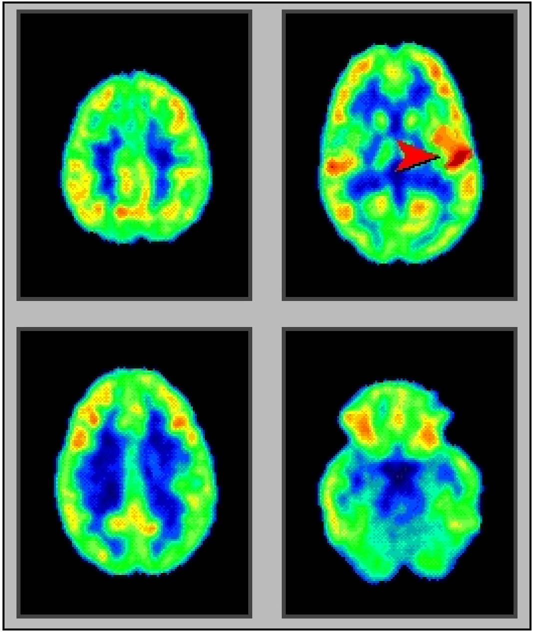


look

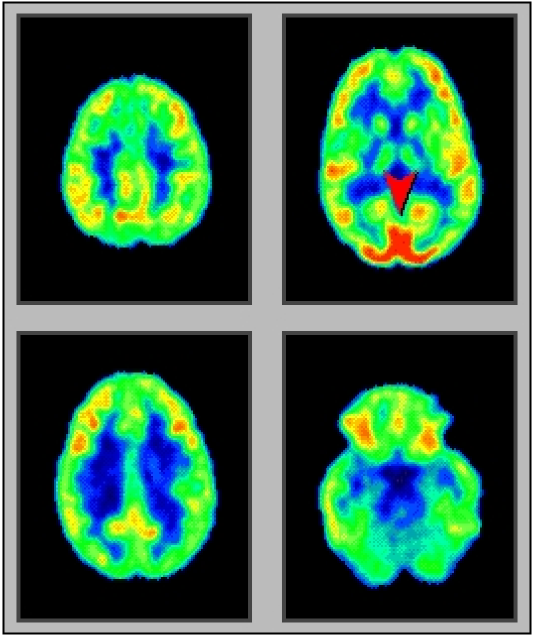
Brain at rest



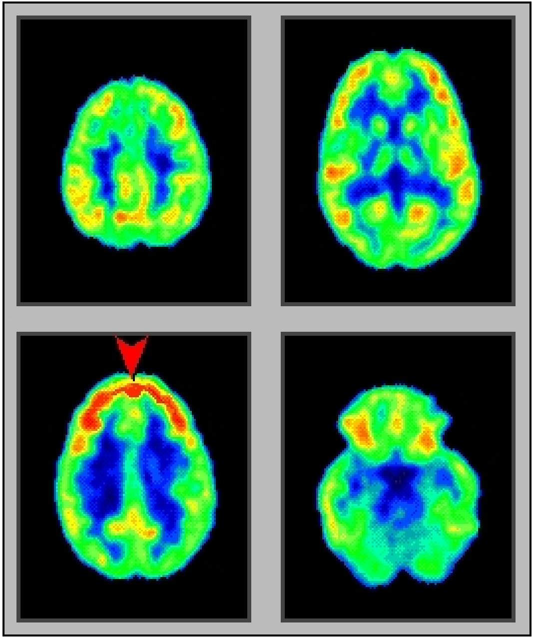
Acoustic stimulation



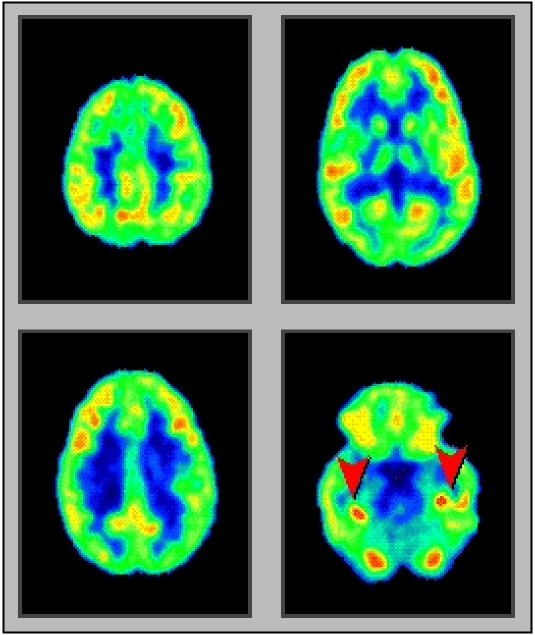
Visual stimulation



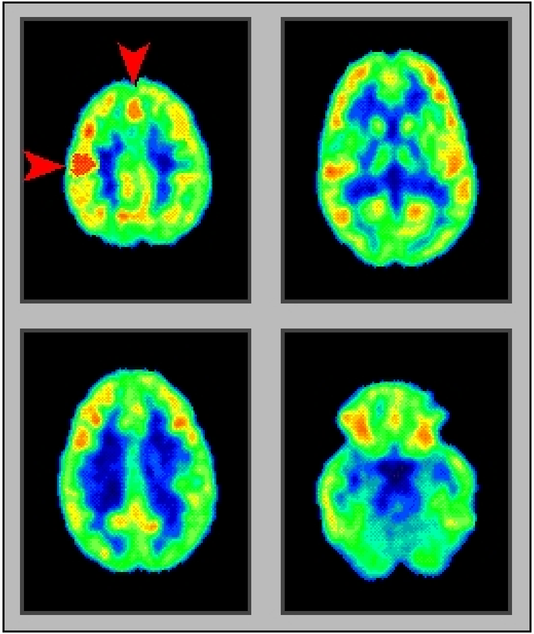
Cognitive activity



Memory and learning

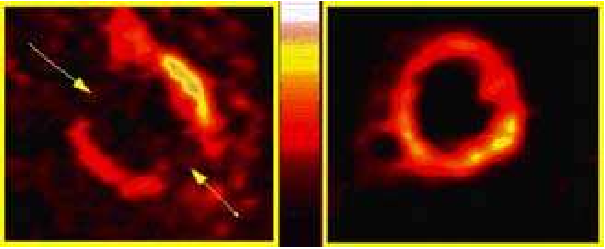


Movement



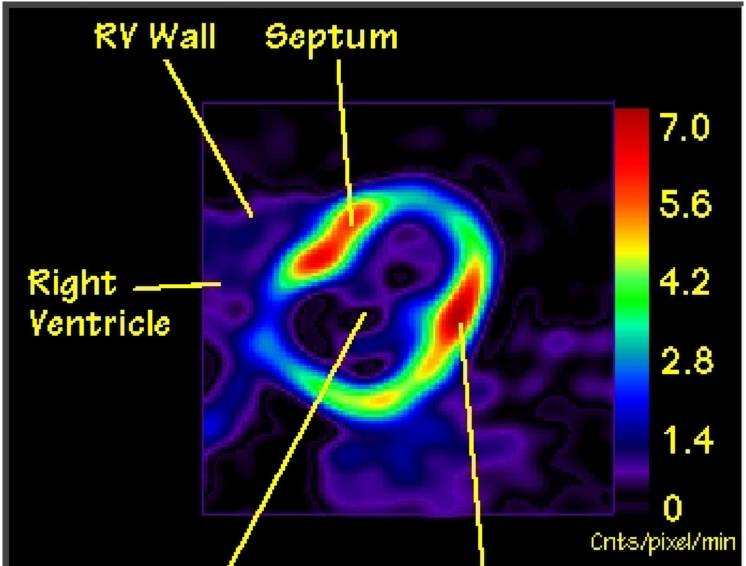
PET: Applications

Cardiac imaging



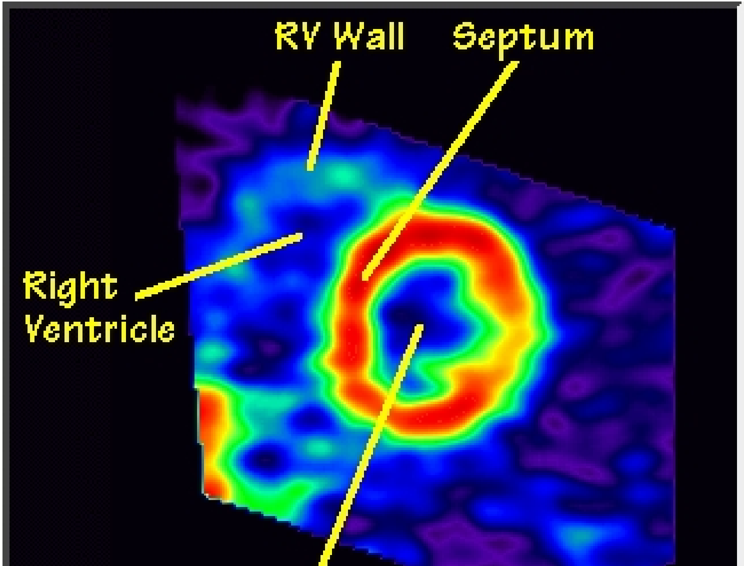
PET, heart

Contrast agent FDG

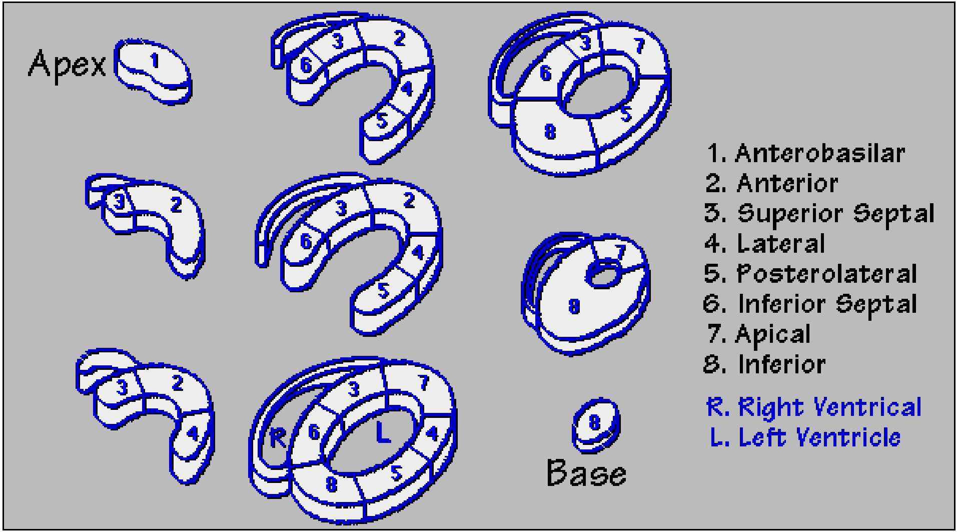


PET, heart

Contrast agent FDG

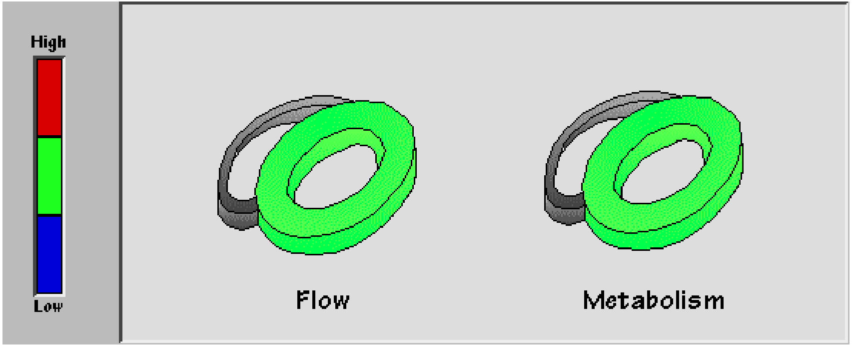


Heart segments



Heart diagnostics

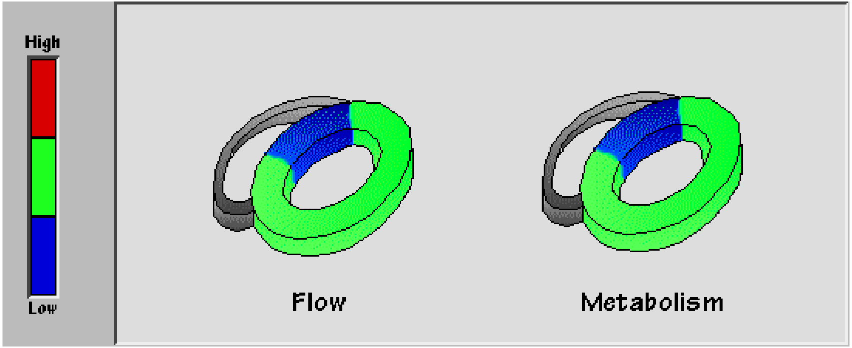
Flow (e.g. NH_3) Metabolism (e.g. FDG)



Normal

Heart diagnostics

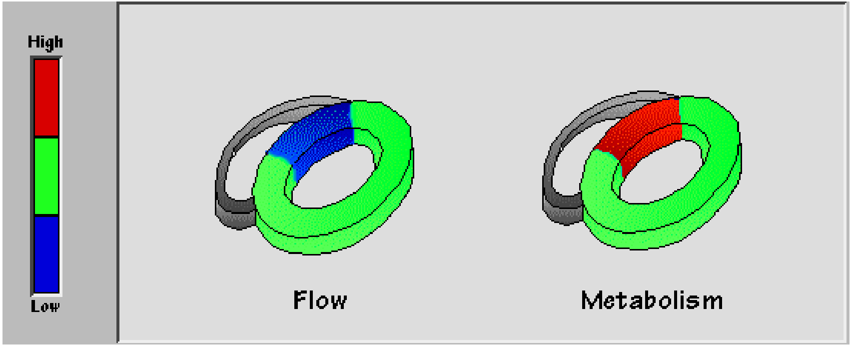
Flow (e.g. NH_3)   Metabolism (e.g. FDG)



Not functional tissue, treatment not possible.

Heart diagnostics

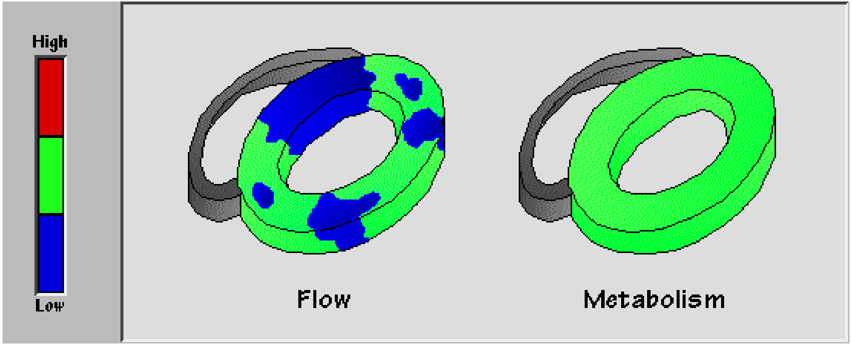
Flow (e.g. NH_3) Metabolism (e.g. FDG)



Insufficient perfusion, treatment possible.

Heart diagnostics

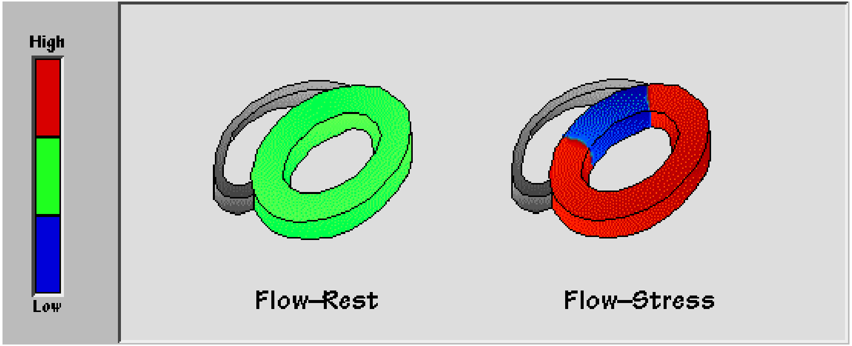
Flow (e.g. NH_3)   Metabolism (e.g. FDG)



Bad perfusion (ischemic), enlarged myocardium. Treatment possible if the metabolism is normal or increased.

Heart diagnostics

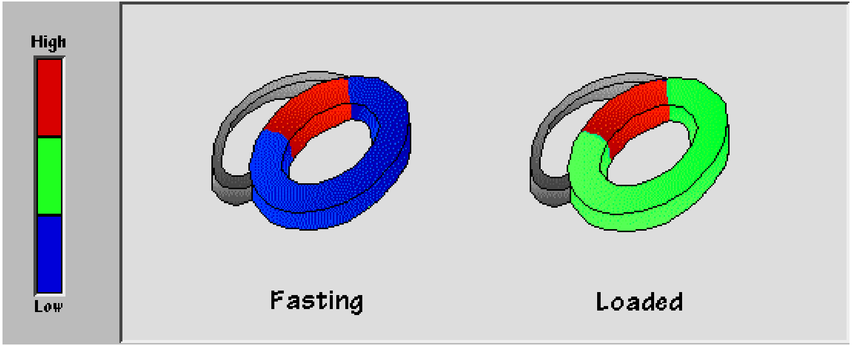
Flow (e.g. NH_3) Metabolism (e.g. FDG)



Bad perfussion after load test.

Heart diagnostics

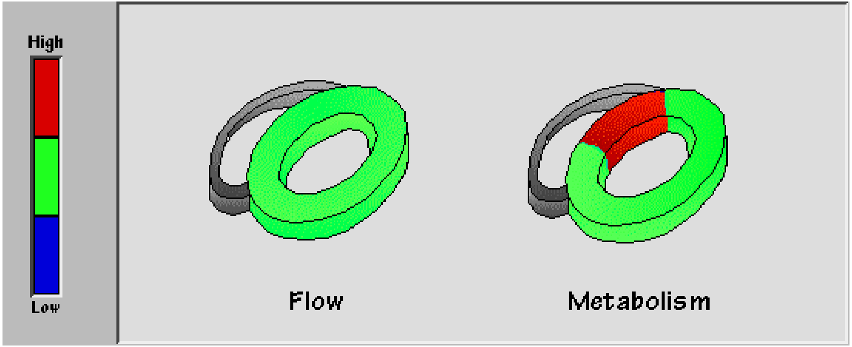
Flow at rest   Flow at load



Ischemic myocardium needs more glucose.

Heart diagnostics

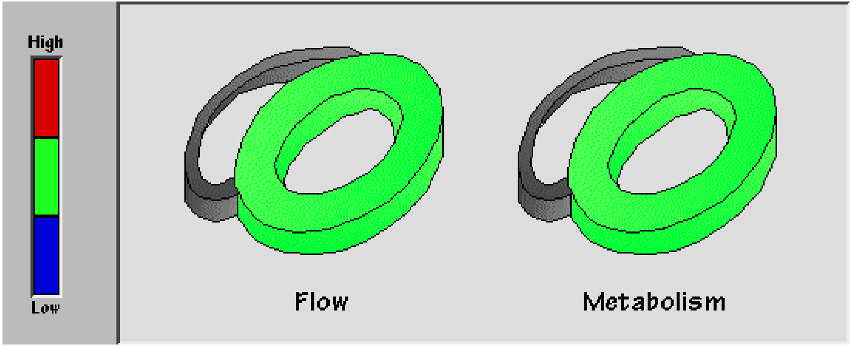
Fasting   After glucose is administerd



Hibernating myocardium.

Heart diagnostics

Flow (e.g. NH_3)   Metabolism (e.g. FDG)



Idiopatically enlarged left ventricle. Only transplantation.

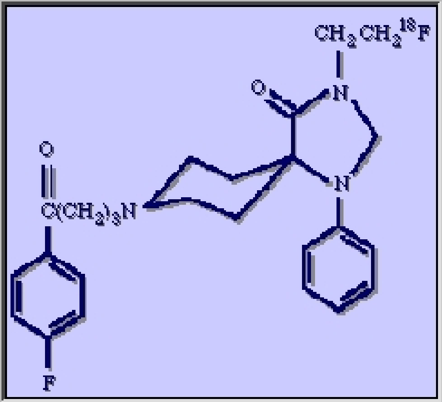
Kinetic study

- Study the evolution of the radiotracer concentration in time
- Identify model parameters (time and transport constants)

Kinetic study

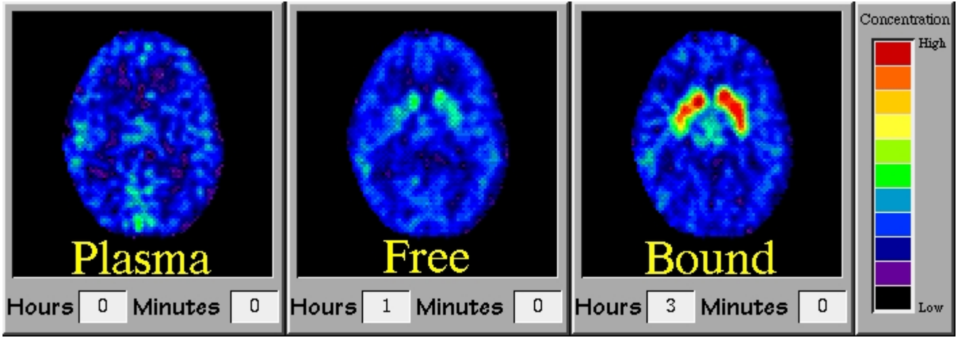
- Study the evolution of the radiotracer concentration in time
- Identify model parameters (time and transport constants)
- $\longrightarrow$ Reproducibility

Brain

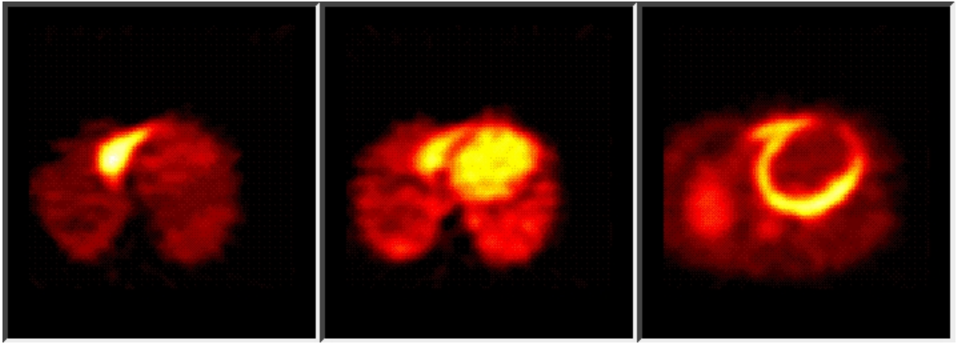


Fluoroethylspiperone

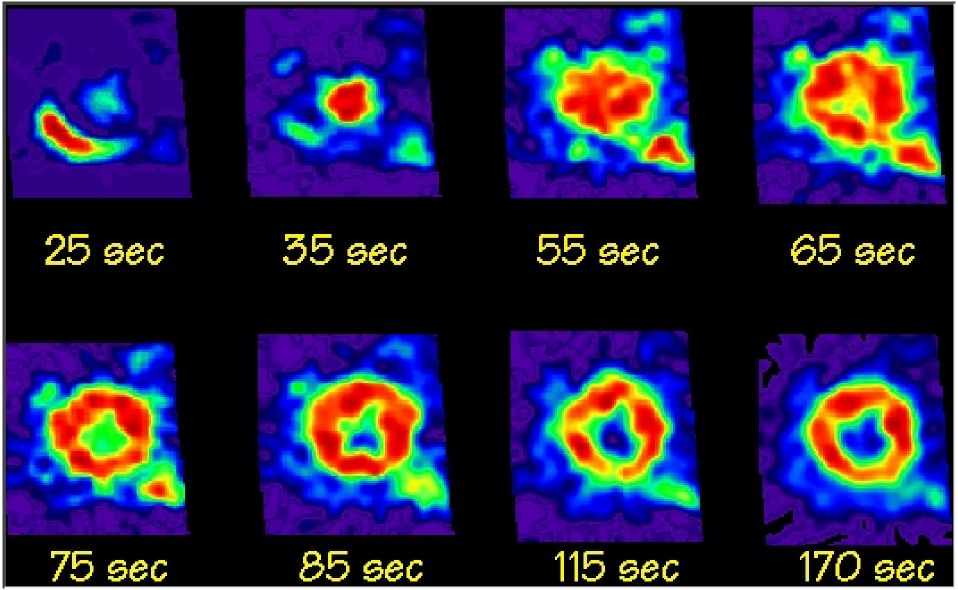
Brain


Plasma
Free
Bound
Hours 0 Minutes 0
Hours 1 Minutes 0
Hours 3 Minutes 0
Concentration
High
Low

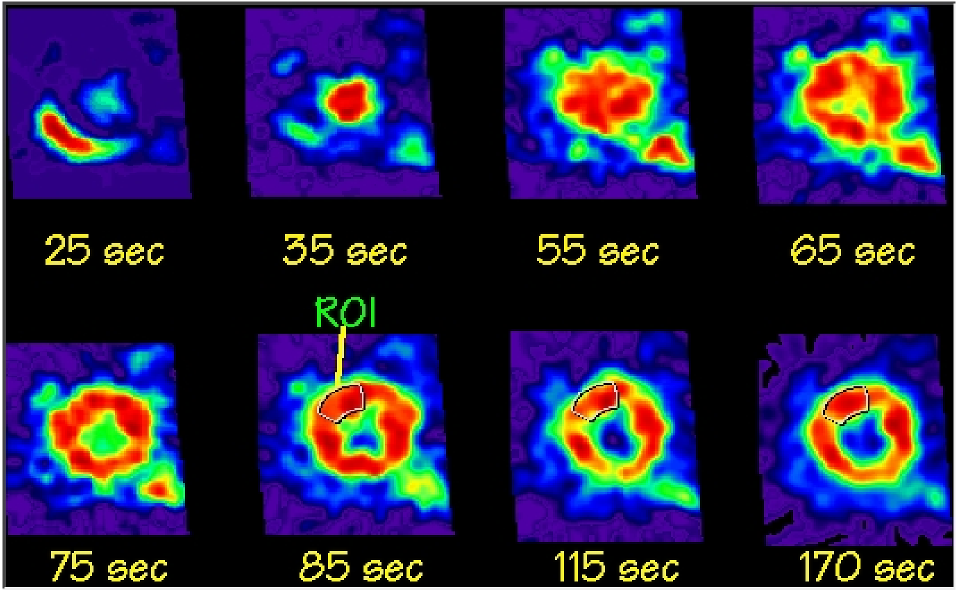
Heart



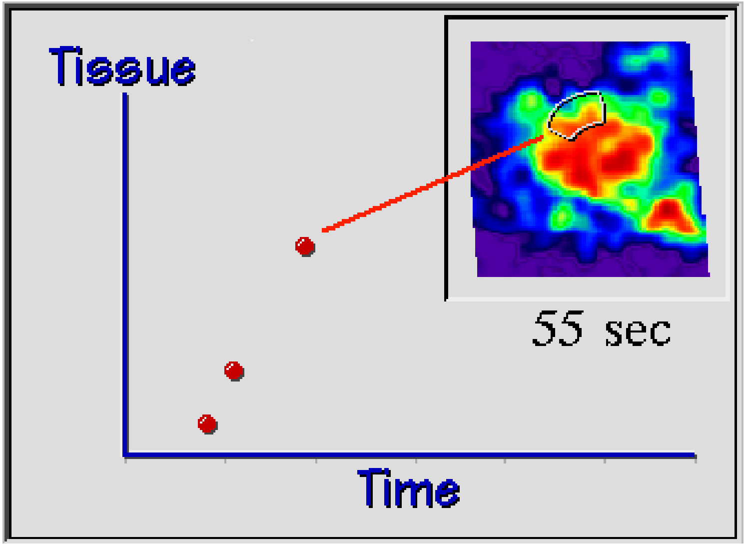
Heart



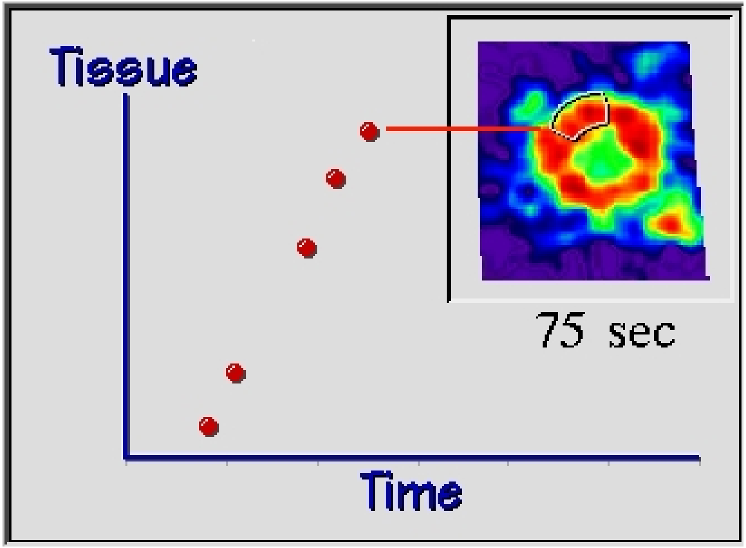
Heart — ROI analysis



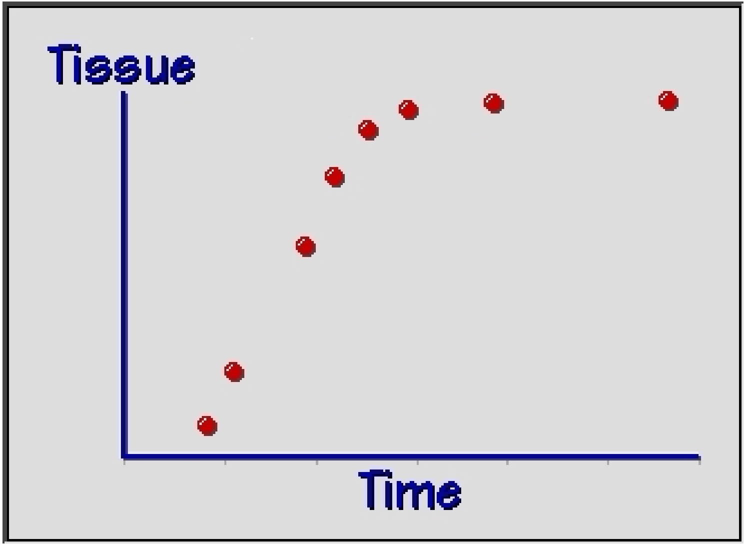
Heart — ROI analysis



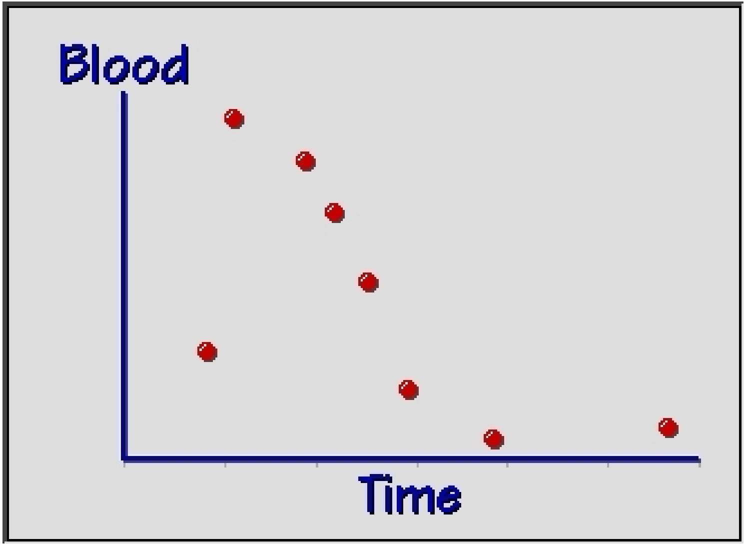
Heart — ROI analysis



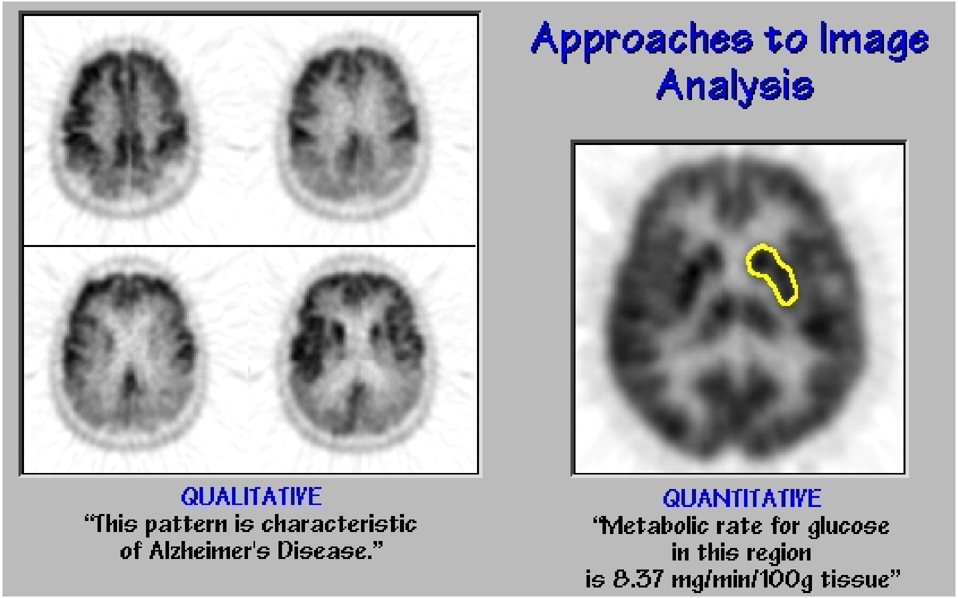
Heart — ROI analysis



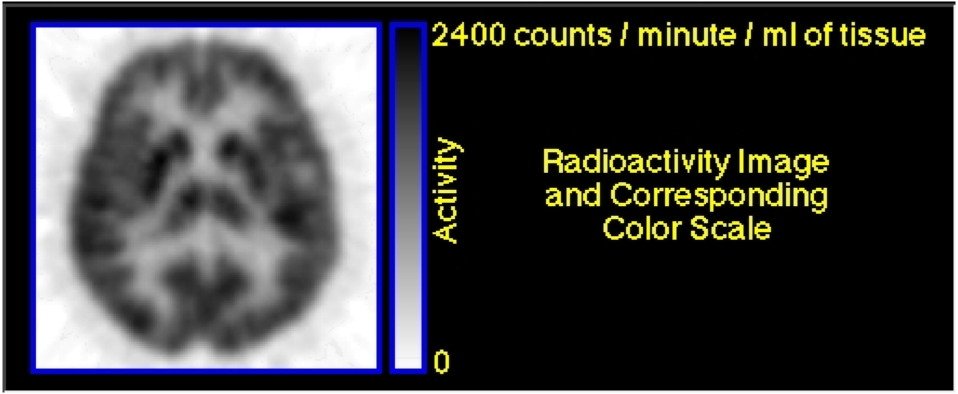
Heart — ROI analysis



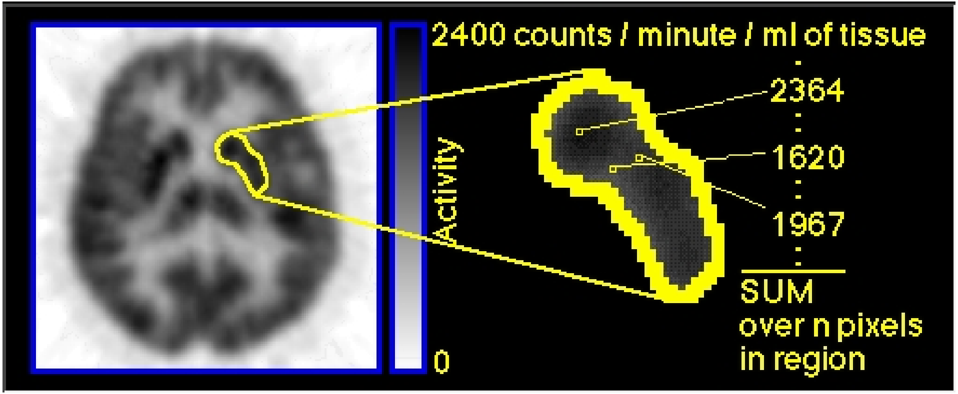
Qualitative × quantitative analysis



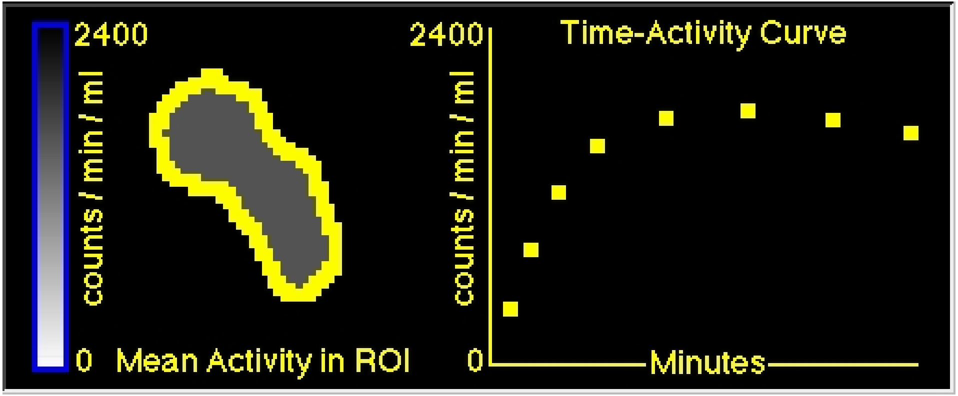
Normalized radioactivity image



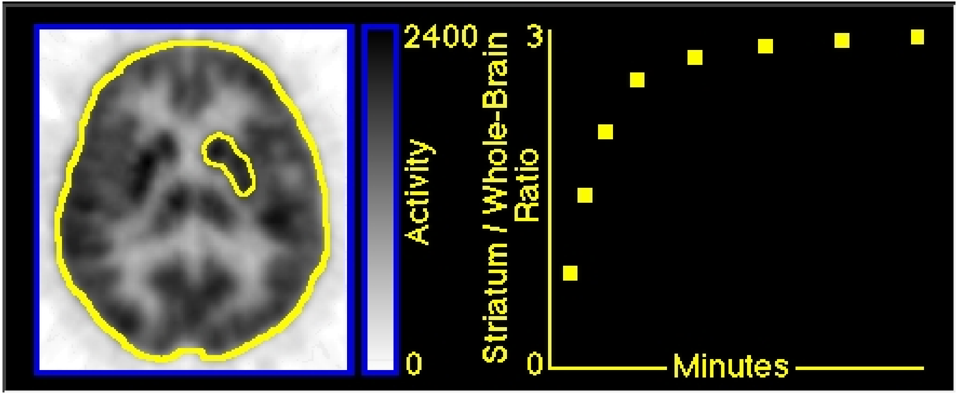
Mean ROI value



Time-activity ROI curve

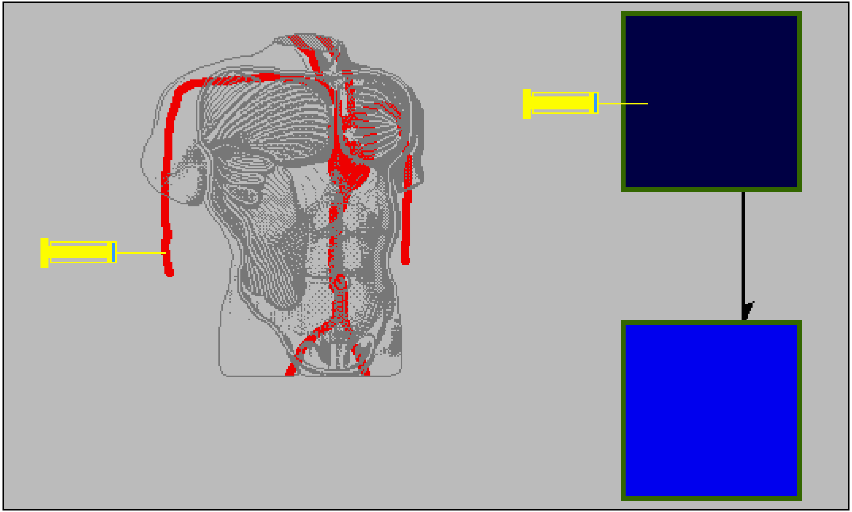


Normalized time-activity ROI curve



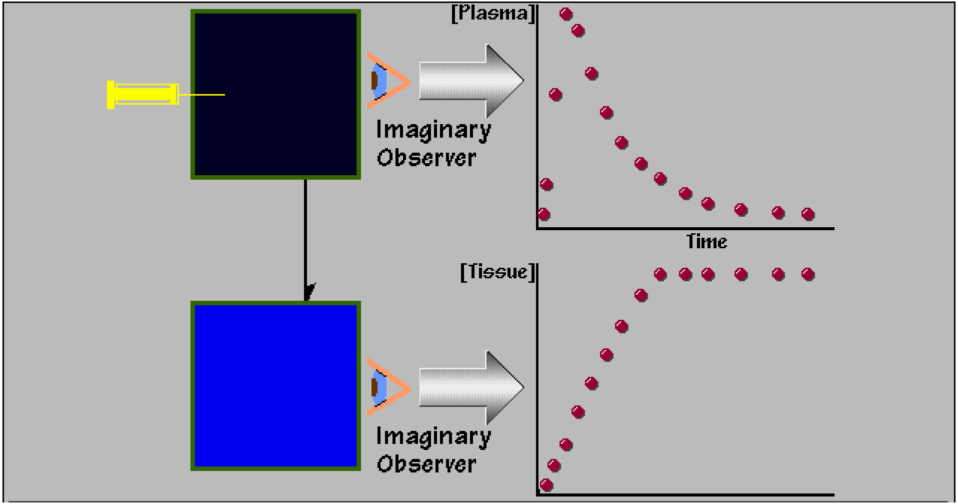
Ratio of regional and total activity.

Tracer modeling of the ROI curve



- Find biophysical model parameters — blood flow, concentrations, diffusion coefficients.

Tracer modeling of the ROI curve



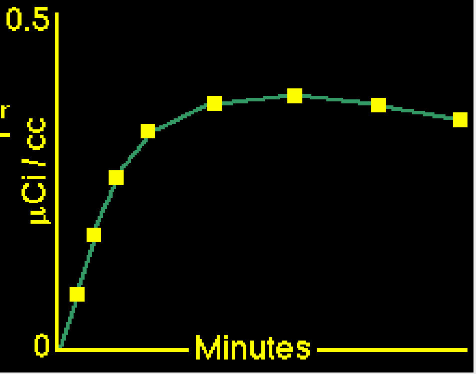
Tracer modeling of the ROI curve

Iteration #: 3

Chi-Square: 0.6879142

Parameter	Estimate	Standard Error
k1	0.1019	0.01735
k2	0.1326	0.02242
k3	0.06548	0.006839

Convergence has occurred.



Nuclear imaging — summary

+ Functional imaging; intensity of the metabolic processes
+ Targeted and specific imaging, perfussion, oncology
- Radiation dose
- Manufacturing radiopharmaceuticals, expensive
- Only partial anatomy information
- Bad spatial resolution